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Maier et al.

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(54) **METHOD AND APPARATUS FOR VIBRATION-RELATED ARTIFACT REDUCTION**

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(51) **Int. Cl.**
G01V 3/00 (2006.01)

(52) **U.S. Cl.** **324/309; 324/307**

(58) **Field of Classification Search** **324/300-322; 600/407-445**

See application file for complete search history.

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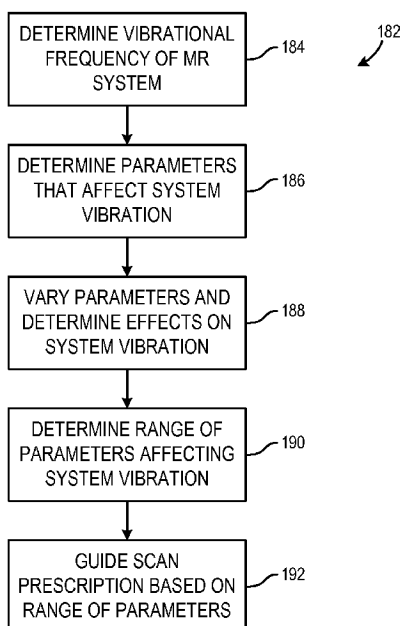
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(57) **ABSTRACT**

A method and apparatus for reducing vibration-related artifacts in diffusion weighted imaging determines a vibrational frequency of an MR system and modifies scan parameters such that vibrational frequencies induced on the MR system are inconsistent with the vibrational frequency of the MR system. The method and apparatus improves image quality of MR images acquired using diffusion weighted imaging techniques with the MR system. As such, modification and/or redesign of the MR system to reduce vibrational frequency interaction is reduced.

21 Claims, 11 Drawing Sheets



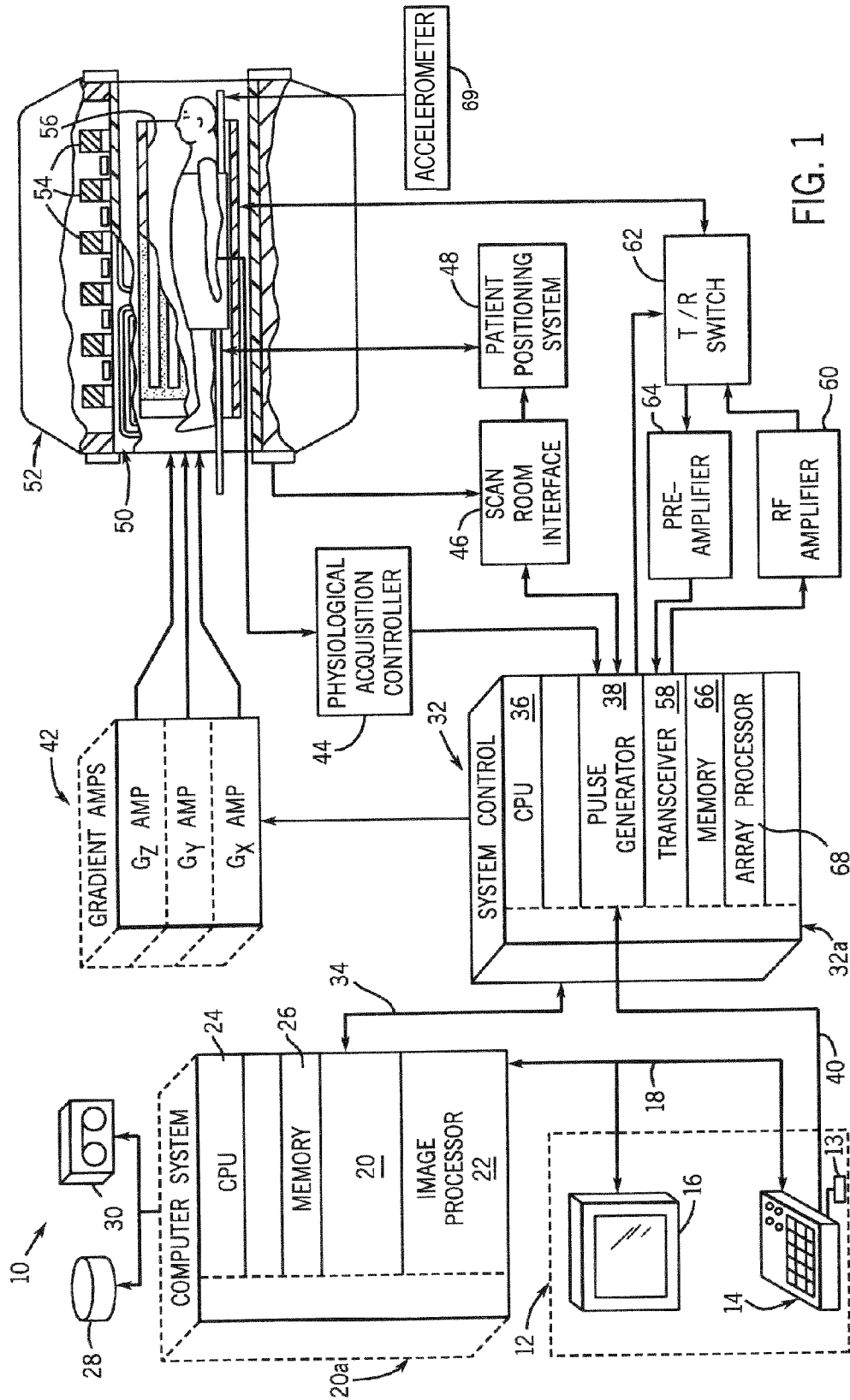


FIG. 1

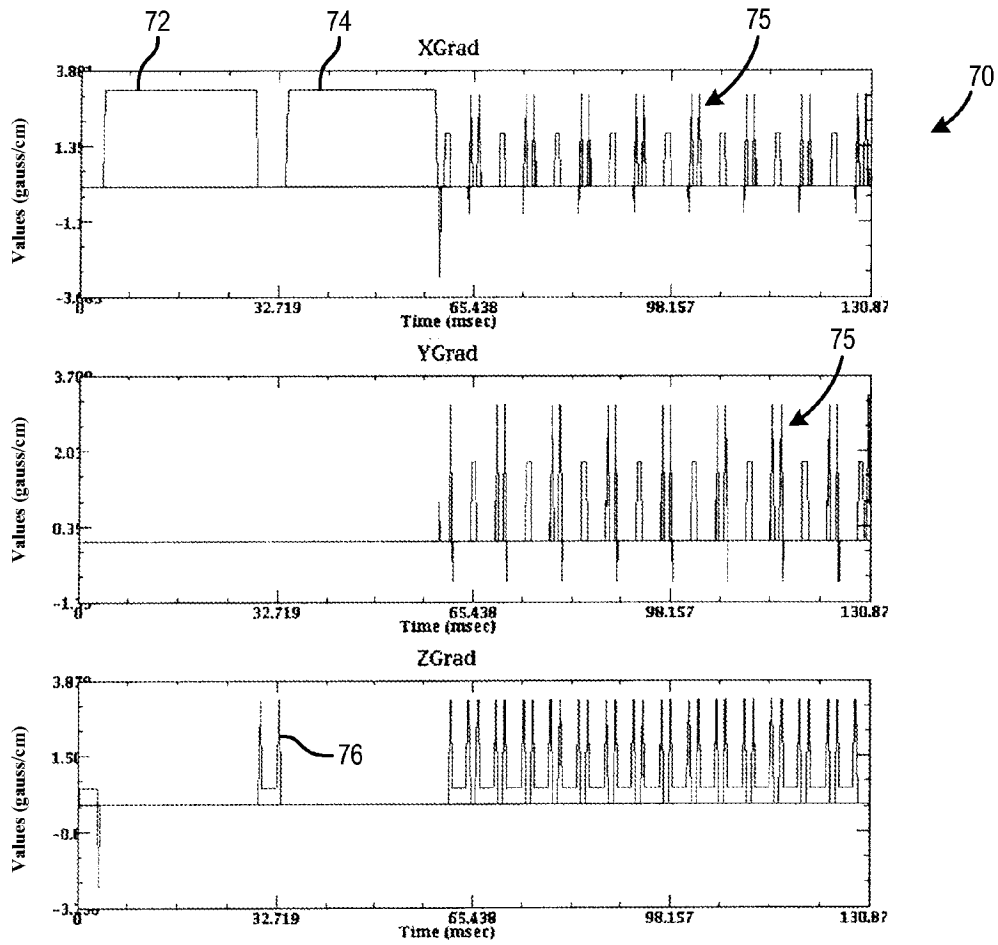


FIG. 2
-PRIOR ART-

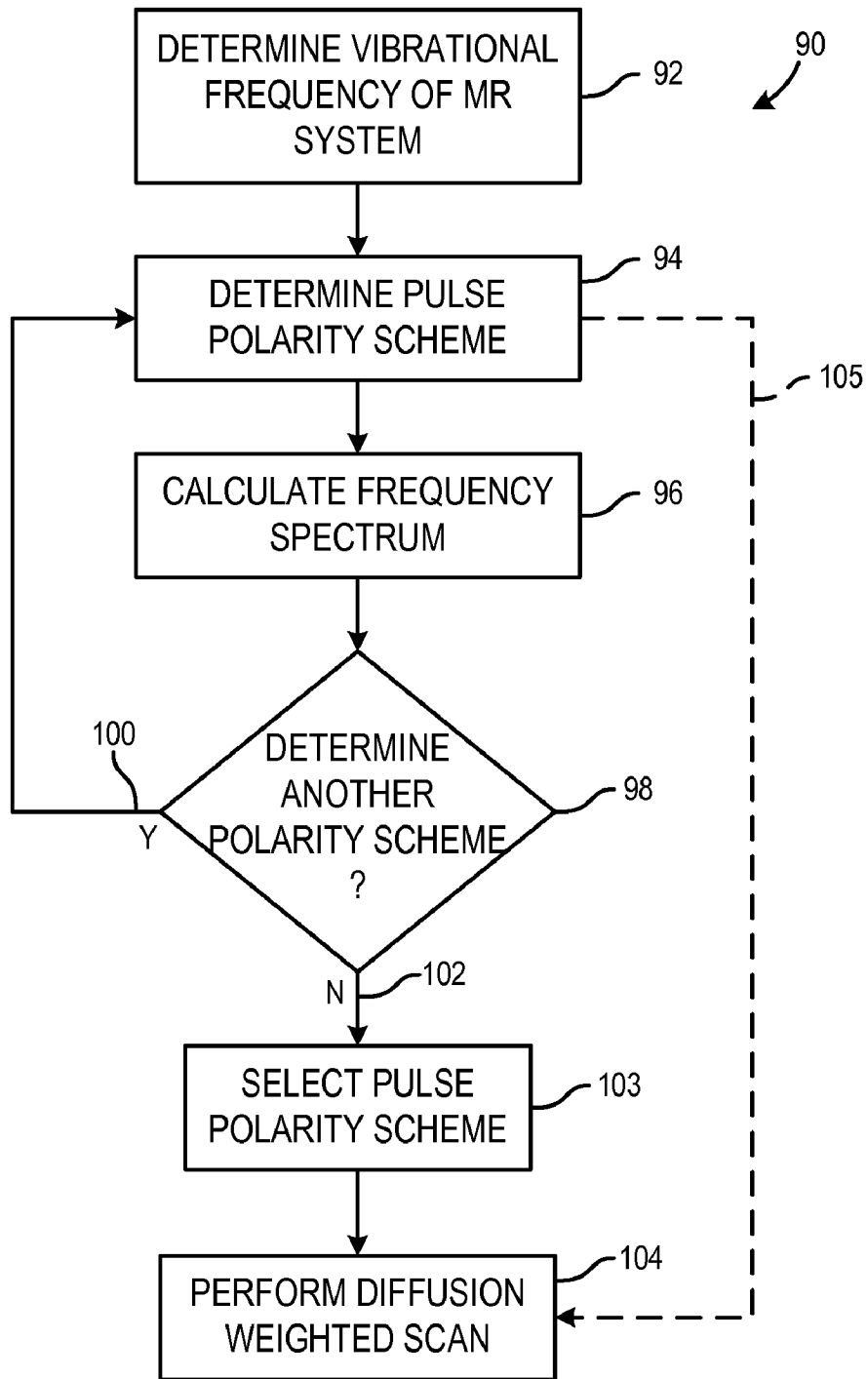


FIG. 3

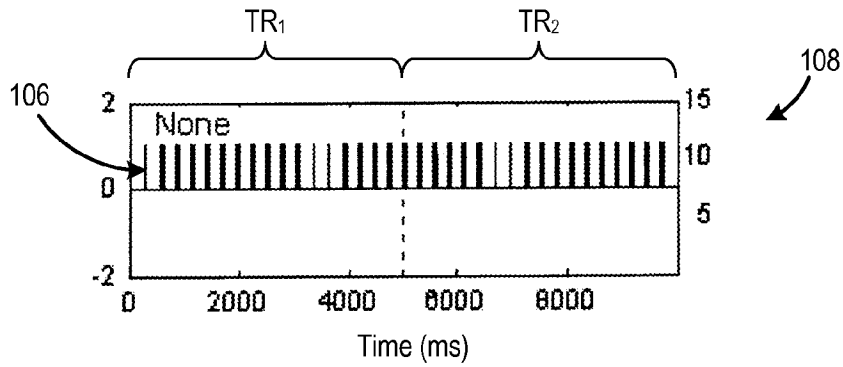


FIG. 4

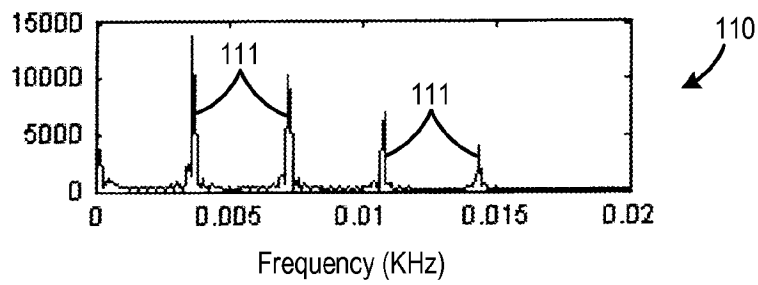


FIG. 5

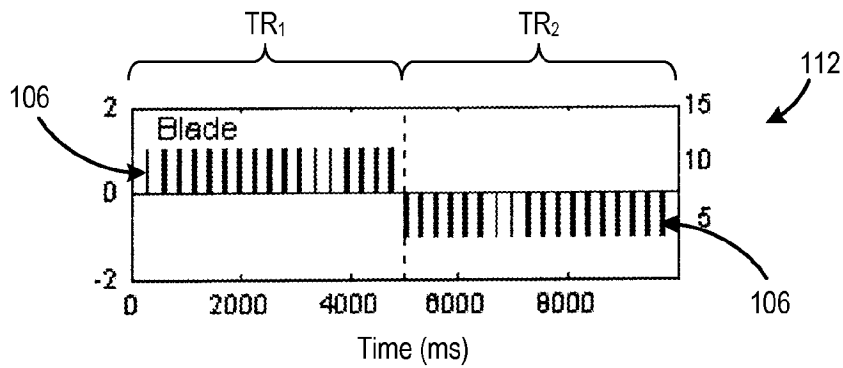


FIG. 6

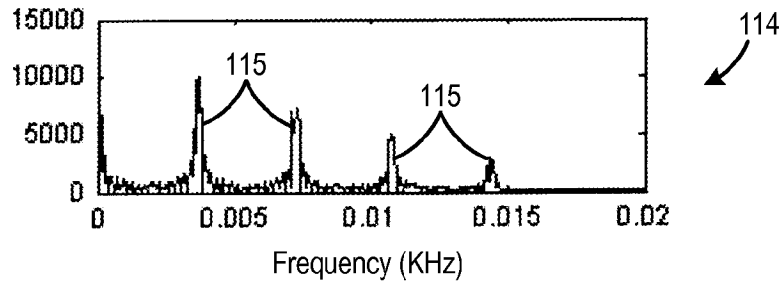


FIG. 7

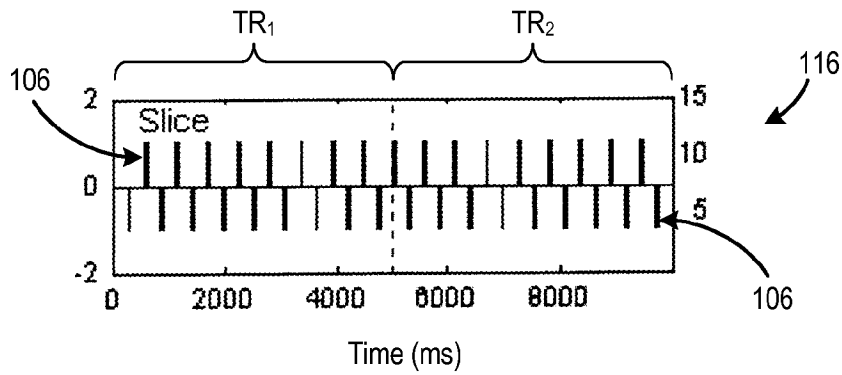


FIG. 8

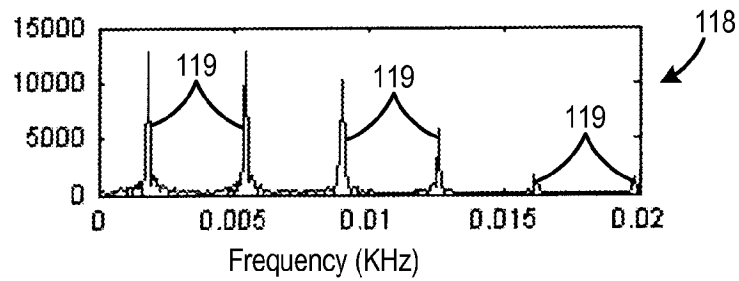


FIG. 9

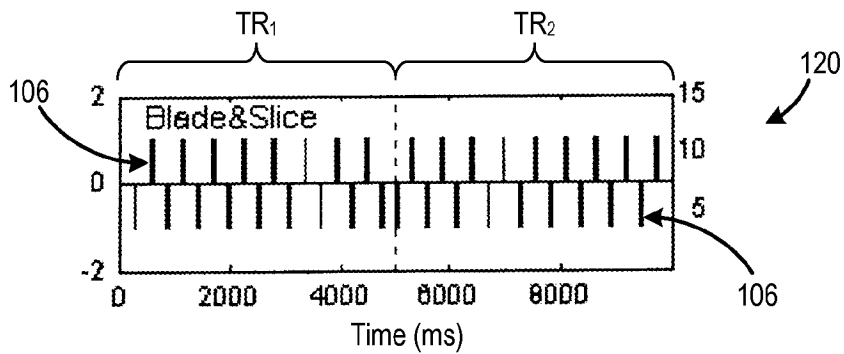


FIG. 10

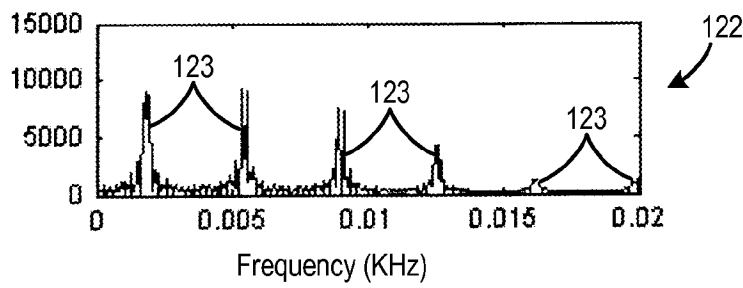


FIG. 11

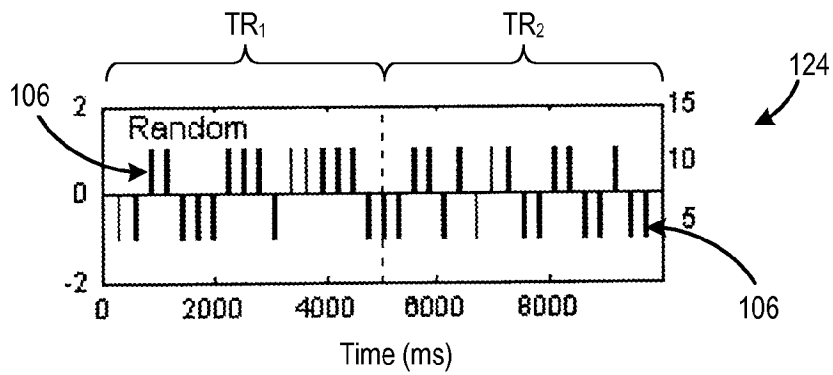


FIG. 12

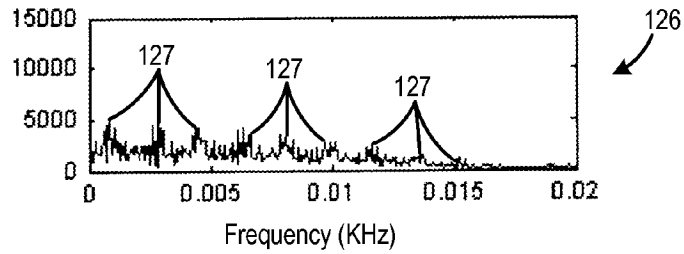


FIG. 13

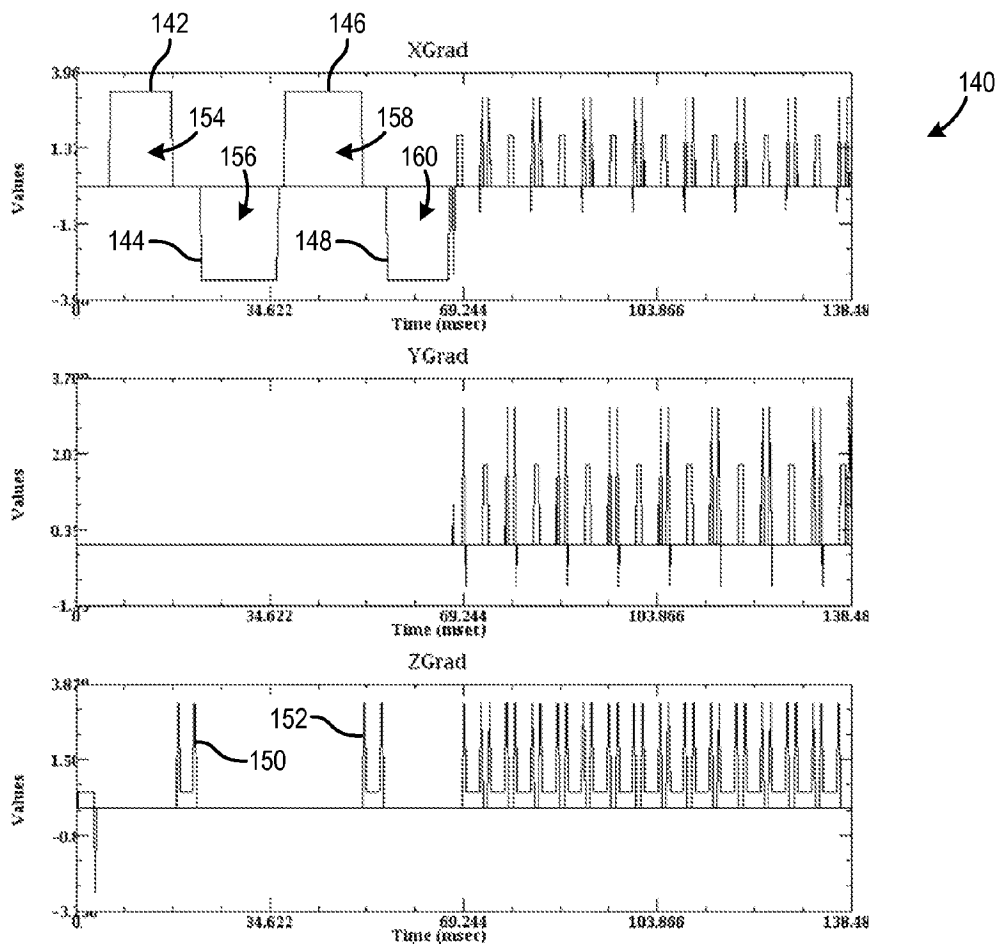


FIG. 14

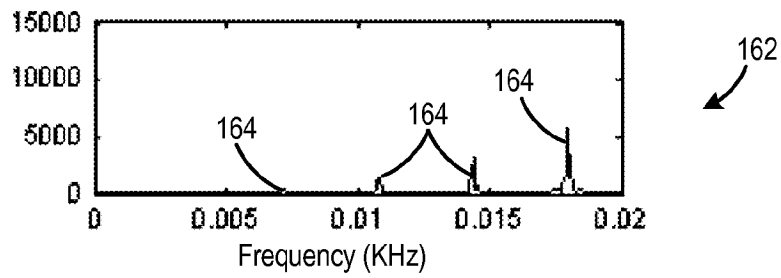


FIG. 15

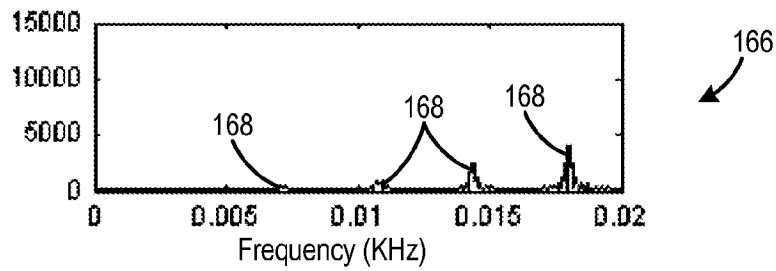


FIG. 16

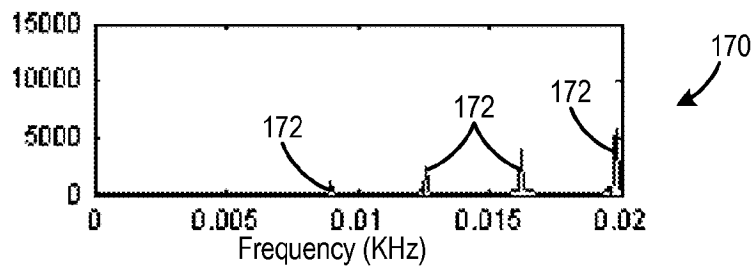


FIG. 17

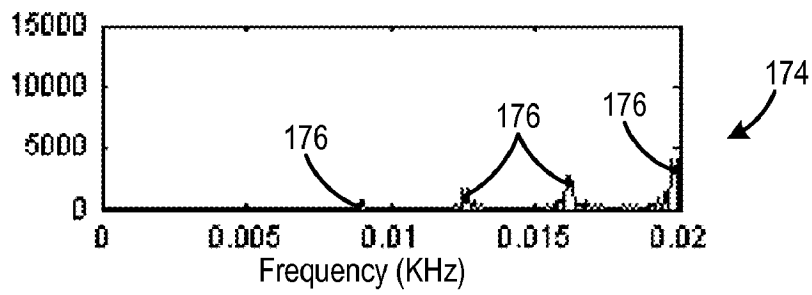


FIG. 18

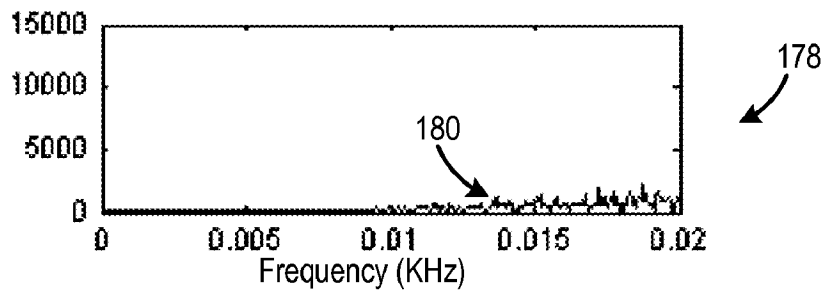


FIG. 19

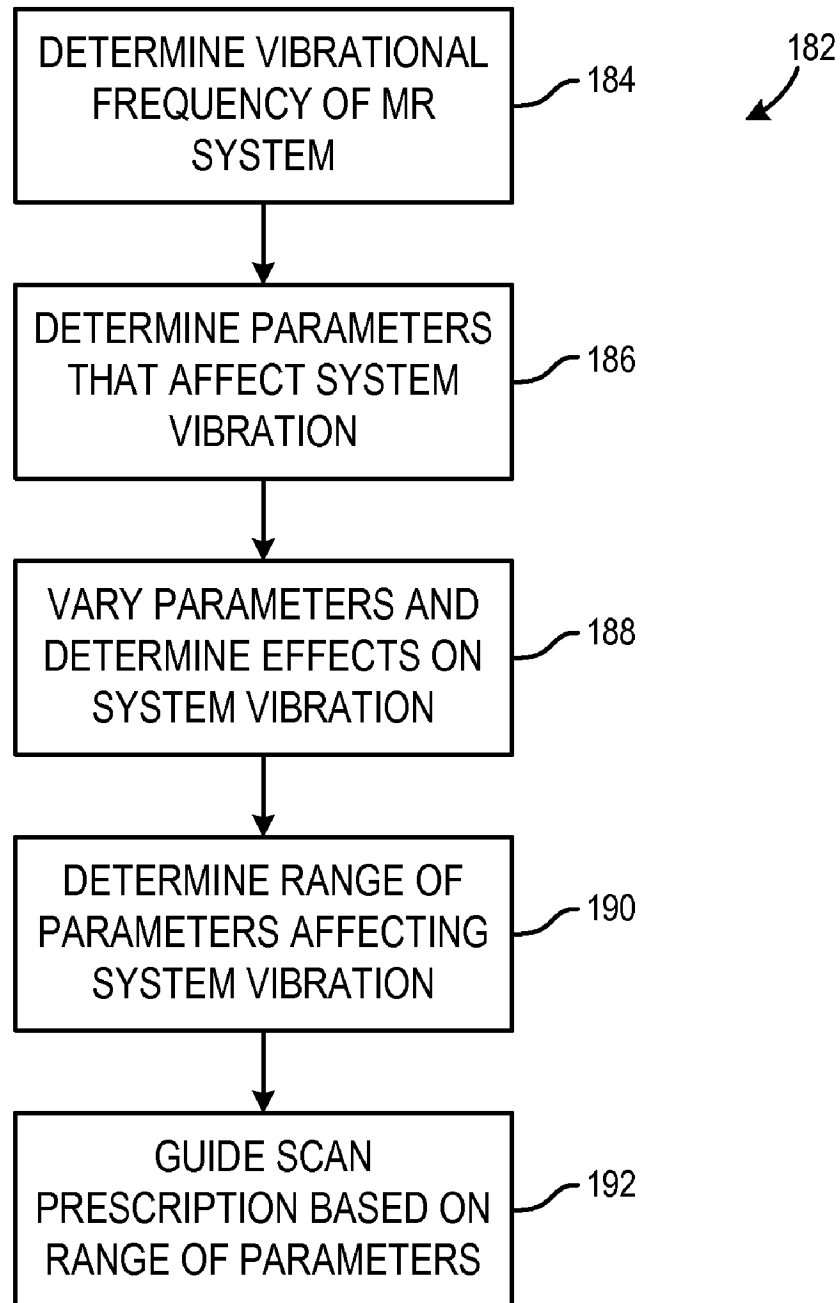


FIG. 20

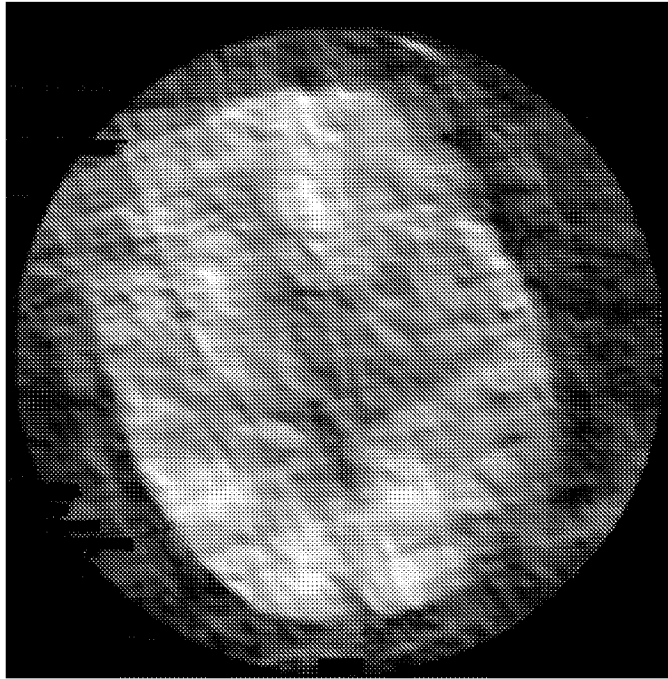


FIG. 21
-PRIOR ART-

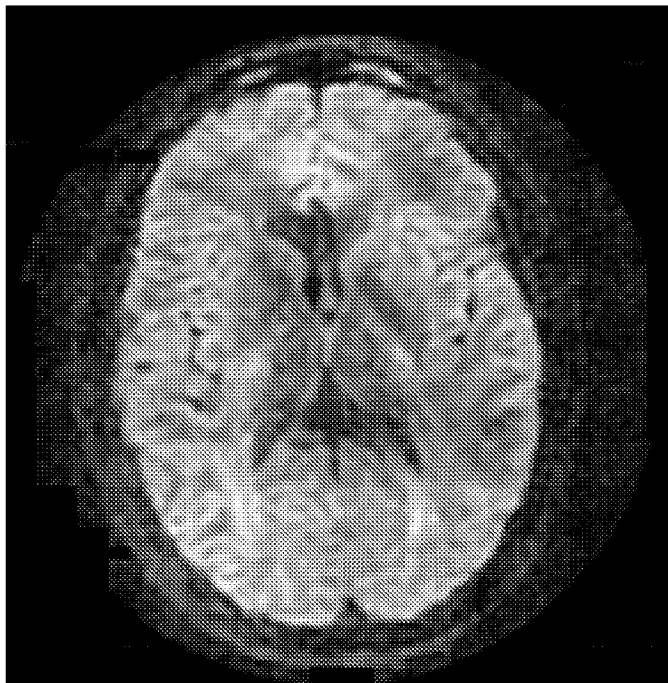


FIG. 22

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METHOD AND APPARATUS FOR VIBRATION-RELATED ARTIFACT REDUCTION

CROSS REFERENCE TO RELATED APPLICATIONS

The present application is a continuation of and claims priority of U.S. Ser. No. 11/275,286 filed Dec. 21, 2005, the disclosure of which is incorporated herein by reference.

BACKGROUND OF THE INVENTION

The present invention relates generally to magnetic resonance (MR) imaging and, more particularly, to reducing vibration-related artifacts in diffusion weighted MR imaging.

When a substance such as human tissue is subjected to a uniform magnetic field (polarizing field B_0), the individual magnetic moments of the spins in the tissue attempt to align with this polarizing field, but precess about it in random order at their characteristic Larmor frequency. If the substance, or tissue, is subjected to a magnetic field (excitation field B_1) which is in the x-y plane and which is near the Larmor frequency, the net aligned moment, or "longitudinal magnetization", M_z , may be rotated, or "tipped", into the x-y plane to produce a net transverse magnetic moment M_r . A signal is emitted by the excited spins after the excitation signal B_1 is terminated and this signal may be received and processed to form an image.

When utilizing these signals to produce images, magnetic field gradients (G_x , G_y , and G_z) are employed. Typically, the region to be imaged is scanned by a sequence of measurement cycles in which these gradients vary according to the particular localization method being used. The resulting set of received NMR signals are digitized and processed to reconstruct the image using one of many well known reconstruction techniques.

As described above, magnetic field gradients are applied in MR imaging to encode spins in an object. It is desirable that the spatial frequency coordinates, i.e., k-space coordinates k_x , k_y , in cycles/cm, of raw data samples acquired during MR imaging be controlled solely via the integrals of the applied encoding gradients. Ideally, these gradients impart directional and linear phase dispersion to the spins inside the object. The raw data's peak occurs at the point where minimal phase dispersion occurs across the object, i.e., when the integrals of the applied gradients go to zero. The gradient waveforms and analog-to-digital conversion are typically synchronized such that the raw data peak location is known with respect to the raw data matrix dimensions.

However, a number of undesirable mechanisms can cause shifts where the peak occurs within the raw data matrix. For example, gradient amplifier infidelity, gradient pulse induced eddy current fields, gradient channel group delays, and pulse sequence database timing errors can cause such shifts. Another undesirable mechanism causes residual phase dispersion across the object where object motion occurs during the application of the gradients. When undesirable mechanisms motion occurs, the phase "unwinding" imparted by a later gradient pulse does not align spatially inside the object with the previous phase "wind up" imparted by an earlier gradient pulse.

The subsequent shift in the raw data peak can be problematic in MR imaging methods where the raw data sampling is stopped or truncated near to the ideal assumed position of the peak and, in particular, diffusion weighted sequences. For example, "fractional k_y " Diffusion Weighted Echo Planar

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Imaging (DWEPI) may be affected where the k_y sampling may be terminated as close as 16 rows below $k_y=0$. Another diffusion weighted technique is Diffusion Weighted Periodically Rotated Overlapping Parallel Line with Enhanced Reconstruction (DW-PROPELLER), and it can be particularly sensitive to k-space center shifts because the blade height, i.e., minor axis direction, is typically 8, leaving only 4 samples above and below the ideal peak. In this manner, the k-space peak does not have to shift far from the blade center along the minor axis before significant low spatial frequency data is lost, i.e., never taken.

The MR imaging methods of DWEPI and DW-PROPELLER typically use two high amplitude, long diffusion sensitizing gradient pulses to attenuate the signal from tissue diffusing along the applied DW gradient. These pulses make the DW sequences particularly sensitive to object motion induced k-space center shifts since the first diffusion pulse imparts a large phase shift (cycles/cm) across the object before the second one "removes" the phase shift, all under the assumption that the object has not moved during the diffusion pulse pair.

The direction and extent of object motion with respect to the applied diffusion gradient direction affects the extent of resulting k-space shifts. Rotational object motion about an axis "A" during application of diffusion pulses on another perpendicular axis "B" can result in an undesirable linear phase dispersion error along axis "B" and the remaining orthogonal axis "C". If axis "B" and/or "C" happen to be image plane encoding axes, i.e., phase or frequency, k-space center shifts can occur. Rotational motion occurring about a physical z (object S/I) axis with DW gradients on physical X (object R/L) axis is problematic for DW-PROPELLER imaging, and shifts along k_{minor} (k_y) are problematic for DWEPI. Object motion can be object derived voluntary/involuntary motion and/or scanner driven involuntary object motion caused by movement or vibration of mechanical components supporting the object such as a head coil, table, etc. Gradient pulse induced forces exerted on the gradient coil assembly can lead to involuntary object motion, which can cause artifacts in DWEPI and DW-PROPELLER imaging.

It would therefore be desirable to have a method and apparatus capable of reducing motion artifacts caused by scanner-induced involuntary object motion.

BRIEF DESCRIPTION OF THE INVENTION

The present invention provides a method and apparatus of reducing vibration-related artifacts that overcome the aforementioned drawbacks. In this regard, the present invention includes a technique modeling vibrational forces induced with a diffusion gradient pulse sequence on an MR system. The polarities of the gradient pulses in the diffusion gradient pulse sequence are determined to avoid induced vibrational frequencies coincident with inherent mechanical resonant vibrational frequencies of the MR system.

In accordance with one aspect of the invention, an MR apparatus includes an MR system having a plurality of gradient coils positioned about a bore of a magnet to impress a polarizing magnetic field. An RF transceiver system and an RF switch are controlled by a pulse module to transmit and receive RF signals to and from an RF coil assembly to acquire MR images. The MR apparatus also includes a computer programmed to determine a mechanical resonant frequency of the MR system and acquire diffusion weighted MR data such that vibration harmonics generated during application of diffusion weighted gradients to acquire the diffusion

weighted MR data do not coincide with the mechanical resonant frequency of the MR system.

In accordance with another embodiment, a method of MR imaging includes the step of determining a plurality of diffusion gradient pulse sequences, each diffusion gradient pulse sequence having a plurality of diffusion weighted gradient pulses. The method also includes the steps of modeling each of the plurality of diffusion gradient pulse sequences with a distinct gradient amplitude and polarity versus time function having a polarity marker for the plurality of diffusion weighted gradient pulses and generating a temporal frequency spectrum of vibrational forces induced with each of the modeled plurality of diffusion gradient pulse sequences. The method further includes selecting a modeled diffusion gradient pulse sequence from the plurality of modeled diffusion gradient pulse sequences having a temporal frequency spectrum dissimilar from a mechanical resonance frequency spectrum of an MR system and applying the selected modeled diffusion gradient pulse sequence in an MR scan.

In accordance with another aspect of the invention, the invention is embodied in a computer program stored on a computer readable storage medium and having instructions which, when executed by a computer, cause the computer to determine a mechanical resonant (vibrational) frequency of an MR apparatus and determine a series of diffusion gradient pulse polarity schemes for diffusion weighted gradients to be applied by gradient coils of the MR apparatus. A frequency spectrum is calculated of vibrational forces induced for each of the diffusion gradient pulse polarity schemes. The instructions further cause the computer to identify a frequency spectrum having at least one spectral peak at a frequency inconsistent with the mechanical vibration frequency of the MR apparatus and perform a diffusion weighted MR scan of an imaging subject with application of diffusion weighted gradients being governed by the diffusion gradient pulse polarity scheme corresponding to the identified frequency spectrum.

In accordance with yet another aspect of the invention, a method of MR imaging includes the steps of measuring a mechanical resonant frequency of an MR scanner and determining a range of parameters whose corresponding pulse sequence has a gradient sequence that excites the mechanical resonant frequencies of the MR scanner during an MR scan. The use of the MR scanner is limited based on the determined range of parameters.

Various other features and advantages of the present invention will be made apparent from the following detailed description and the drawings.

BRIEF DESCRIPTION OF THE DRAWINGS

The drawings illustrate one preferred embodiment presently contemplated for carrying out the invention.

In the drawings:

FIG. 1 is a schematic block diagram of an MR imaging system for use with the present invention.

FIG. 2 is a portion of a known Single Spin Echo (SSE) DW-PROPELLER pulse sequence to acquire diffusion weighted MR images.

FIG. 3 is a technique for reducing vibration-related artifacts according to the present invention.

FIG. 4 is a gradient pulse polarity scheme for use in the technique of FIG. 3 in accordance with one aspect of the invention.

FIG. 5 is a frequency spectrum corresponding to a Fourier transform of the gradient pulse polarity scheme of FIG. 4 applied to SSE diffusion gradients.

FIG. 6 is a gradient pulse polarity scheme for use in the technique of FIG. 3 in accordance with another aspect of the invention.

FIG. 7 is a frequency spectrum corresponding to a Fourier transform of the gradient pulse polarity scheme of FIG. 6 applied to SSE diffusion gradients.

FIG. 8 is a gradient pulse polarity scheme for use in the technique of FIG. 3 in accordance with a further aspect of the invention.

FIG. 9 is a frequency spectrum corresponding to a Fourier transform of the gradient pulse polarity scheme of FIG. 8 applied to SSE diffusion gradients.

FIG. 10 is a gradient pulse polarity scheme for use in the technique of FIG. 3 in accordance with another aspect of the invention.

FIG. 11 is a frequency spectrum corresponding to a Fourier transform of the gradient pulse polarity scheme of FIG. 10 applied to SSE diffusion gradients.

FIG. 12 is a gradient pulse polarity scheme for use in the technique of FIG. 3 in accordance with another aspect of the invention.

FIG. 13 is a frequency spectrum corresponding to a Fourier transform of the gradient pulse polarity scheme of FIG. 12 applied to SSE diffusion gradients.

FIG. 14 is a portion of a Dual Spin Echo (DSE) DW-PROPELLER pulse sequence to acquire diffusion weighted MR images.

FIG. 15 is a frequency spectrum corresponding to a Fourier transform of the gradient pulse polarity scheme of FIG. 4 applied to DSE diffusion gradients.

FIG. 16 is a frequency spectrum corresponding to a Fourier transform of the gradient pulse polarity scheme of FIG. 6 applied to DSE diffusion gradients.

FIG. 17 is a frequency spectrum corresponding to a Fourier transform of the gradient pulse polarity scheme of FIG. 8 applied to DSE diffusion gradients.

FIG. 18 is a frequency spectrum corresponding to a Fourier transform of the gradient pulse polarity scheme of FIG. 10 applied to DSE diffusion gradients.

FIG. 19 is a frequency spectrum corresponding to a Fourier transform of the gradient pulse polarity scheme of FIG. 12 applied to DSE diffusion gradients.

FIG. 20 is another technique for reducing vibration-related artifacts according to the present invention.

FIG. 21 is a reconstructed image acquired from a known diffusion weighted imaging technique.

FIG. 22 is a reconstructed image from a diffusion weighted imaging technique according to the present invention.

DETAILED DESCRIPTION OF THE PREFERRED EMBODIMENT

Referring to FIG. 1, the major components of a preferred MR system 10 incorporating the present invention are shown. The operation of the system is controlled from an operator console 12 which includes a keyboard or other input device 13, a control panel 14, and a display screen 16. The console 12 communicates through a link 18 with a separate computer system 20 that enables an operator to control the production and display of images on the display screen 16. The computer system 20 includes a number of modules which communicate with each other through a backplane 20a. These include an image processor module 22, a CPU module 24 and a memory module 26, known in the art as a frame buffer for storing image data arrays. The computer system 20 is linked to disk storage 28 and tape drive 30 or other storage medium for storage of image data and programs, and communicates with

a separate system control **32** through a high speed serial link **34**. The input device **13** can include a mouse, joystick, keyboard, track ball, touch activated screen, light wand, voice control, or any similar or equivalent input device, and may be used for interactive geometry prescription.

The system control **32** includes a set of modules connected together by a backplane **32a**. These include a CPU module **36** and a pulse generator module **38** which connects to the operator console **12** through a serial link **40**. It is through link **40** that the system control **32** receives commands from the operator to indicate the scan sequence that is to be performed. The pulse generator module **38** operates the system components to carry out the desired scan sequence and produces data which indicates the timing, strength and shape of the RF pulses produced, and the timing and length of the data acquisition window. The pulse generator module **38** connects to a set of gradient amplifiers **42**, to indicate the timing and shape of the gradient pulses that are produced during the scan. The pulse generator module **38** can also receive object data, i.e., of an object, from a physiological acquisition controller **44** that receives signals from a number of different sensors connected to the object, such as ECG signals from electrodes attached to the object. And finally, the pulse generator module **38** connects to a scan room interface circuit **46** which receives signals from various sensors associated with the condition of the object and the magnet system. It is also through the scan room interface circuit **46** that an object positioning system **48** receives commands to move the object to the desired position for the scan.

The gradient waveforms produced by the pulse generator module **38** are applied to the gradient amplifier system **42** having G_x, G_y, and G_z amplifiers. Each gradient amplifier excites a corresponding physical gradient coil in a gradient coil assembly generally designated **50** to produce the magnetic field gradients used for spatially encoding acquired signals. The gradient coil assembly **50** forms part of a magnet assembly **52** which includes a polarizing magnet **54** and a whole-body RF coil **56**. A transceiver module **58** in the system control **32** produces pulses which are amplified by an RF amplifier **60** and coupled to the RF coil **56** by a transmit/receive switch **62**. The resulting signals emitted by the excited nuclei in the object may be sensed by the same RF coil **56** and coupled through the transmit/receive switch **62** to a preamplifier **64**. The amplified MR signals are demodulated, filtered, and digitized in the receiver section of the transceiver **58**. The transmit/receive switch **62** is controlled by a signal from the pulse generator module **38** to electrically connect the RF amplifier **60** to the coil **56** during the transmit mode and to connect the preamplifier **64** to the coil **56** during the receive mode. The transmit/receive switch **62** can also enable a separate RF coil (for example, a surface coil) to be used in either the transmit or receive mode.

The MR signals picked up by the RF coil **56** are digitized by the transceiver module **58** and transferred to a memory module **66** in the system control **32**. A scan is complete when an array of raw k-space data has been acquired in the memory module **66**. This raw k-space data is rearranged into separate k-space data arrays for each image to be reconstructed, and each of these is input to an array processor **68** which operates to Fourier transform the data into an array of image data. This image data is conveyed through the serial link **34** to the computer system **20** where it is stored in memory, such as disk storage **28**. In response to commands received from the operator console **12**, this image data may be archived in long term storage, such as on the tape drive **30**, or it may be further processed by the image processor **22** and conveyed to the operator console **12** and presented on the display **16**.

The MR system **10** can induce involuntary object motion during operation due to application of current through components thereof. For example, the application of pulses in the gradient coil assembly **50** and the RF coil **56** exerts vibrational forces on the MR system **10**. Operational vibration forces of the MR system **10** may be determined by attaching an accelerometer **69** thereto and recording the results. The results may be stored in a lookup table for a particular MR system or for a class of MR systems. The results may also be measured in real-time. A frequency analysis of the MR system **10** may be determined thereby that indicates the vibrational frequencies of the MR system **10**. In particular, the frequency analysis may indicate a peak frequency in which an object is most subject to involuntary motion.

The present invention is directed to a method of reducing vibration-related artifacts that can be carried out on the MR apparatus of FIG. 1, or equivalents thereof. As will be described, the invention is effective in reducing involuntary object motion induced by vibrational forces exerted during application of diffusion gradient pulses. In this regard, the present invention improves image quality and, as such, is believed to be effective in reducing the number of repeat scans that are required of a subject.

Referring now to FIG. 2, a portion of an exemplary known Single Spin Echo (SSE) DW-PROPELLER pulse sequence to acquire diffusion weighted MR images is shown. A diffusion gradient pulse sequence **70** includes two diffusion gradient pulses **72, 74**. In a preferred embodiment, pulse **72** is applied before a slice selective pulse **76**, and pulse **74** is applied after the slice selective pulse **76**. As shown, diffusion gradient pulses **72, 74** are applied along an x axis for each image slice; however, it is contemplated that diffusion gradient pulses **72, 74** may be similarly applied along other axes, such as a y axis or a z axis. For example, the pulses **75** rotate between the x and y gradients to get the different "blades" to rotate, while the diffusion sensitizing pulse pair **72, 74** remains along the x direction. As shown in FIG. 2, pulses **72, 74** each have a positive polarity. That is, the direction of current passing through the gradient coil assembly **50** of FIG. 1 during application of pulses **72, 74** is positive. However, in some diffusion weighted sequences, the polarity of pulses **72, 74** may be negative. Whether positive or negative, both pulses **72, 74** of known diffusion weighted pulse sequences have the same polarity.

Application of pulses **72, 74** induces vibrational forces on the gradient coil assembly **50** of the MR system **10**. Reduction of vibrational frequencies according to the present invention includes determining characteristic resonant vibrational frequencies of the MR system **10** and determining the driver or "applied hammer" frequency characteristic applied to the gradient coil assembly **50** by a particular gradient sequence. In this manner, driver vibrational frequencies of the gradient coil assembly **50** may be compared with the resonant vibrational frequencies of the MR system **10** to find inconsistent peak frequencies therebetween. As will be shown, the driver vibrational frequencies of the gradient coil assembly **50** vary according to the polarity scheme of the diffusion gradient pulses **72, 74** applied thereto.

FIG. 3 shows a vibration-related artifact reducing technique according to the present invention. Technique **90** begins at step **92** by determining a peak vibrational frequency of an MR system **10** without application of diffusion gradients. In a preferred embodiment, the peak vibrational frequency is determined by real-time measurement, or, alternatively, by setting the vibrational frequency equal to a predetermined value such as 10 Hz, for example. Alternatively, the predetermined value may be acquired from a lookup table specific to

the MR system **10** or related to the class of MR systems to which the MR system **10** belongs. Next, a pulse polarity scheme is determined at step **94**. The pulse polarity scheme establishes the polarities for diffusion weighted gradient pulses in a diffusion gradient pulse sequence. In a preferred embodiment, the pulse polarity scheme is a gradient amplitude versus time function for a diffusion gradient pulse sequence over a $2*TR$ interval. However, the pulse polarity scheme may be determined for any number of TR intervals. After the pulse polarity scheme is determined **94**, a frequency spectrum is calculated for the pulse polarity scheme at step **96**. A Fourier transform is applied to the pulse polarity scheme to obtain a magnitude versus frequency spectrum. That is, the Fourier transform calculates vibrational frequencies of the vibrational forces induced with the gradient coil assembly **50** by application of the diffusion gradient pulses of the pulse polarity scheme therewith. Exemplary pulse polarity schemes and corresponding frequency spectra are described below.

Technique **90** next determines whether to determine another polarity scheme and corresponding frequency spectrum at step **98**. If so **98**, **100**, technique **90** returns to step **94** and the process proceeds as described above to determine a different pulse polarity scheme. If not **98**, **102**, the frequency spectrum having peak frequencies at frequencies inconsistent with the peak frequency of the MR system **10** is selected. In a preferred embodiment, the determined frequency spectrum has peak frequencies least coincident with the peak frequency of the MR system **10**. In this manner, vibrational forces induced with the gradient coil apparatus **50** that may coincide with the natural resonant frequencies of the MR system **10** are reduced. Next, at step **103**, the pulse polarity scheme corresponding to the determined frequency spectrum is selected and a diffusion weighted scan is performed at step **104** that incorporates the diffusion gradient pulse polarity scheme. For example, the diffusion weighted scan may be a DWEPI scan or a DW-PROPELLER scan. It is contemplated that a computer, i.e., the computer system **20** of FIG. **1**, may be programmed to perform the steps of technique **90**. In particular, the computer may be programmed to automatically determine the frequency spectrum and automatically select the pulse polarity scheme corresponding to the automatically determined frequency spectrum for the pending scan. Alternatively, the computer may be programmed to display the frequency spectrum and receive a user input from an operator indicating a desired selected frequency spectrum and/or pulse polarity scheme for the impending scan.

The peak vibrational frequency of the MR system **10** may vary for each installation of the MR system **10**. That is, an MR system **10** installed at a first site may have a different peak vibrational frequency than a similar MR system installed at a second site. Furthermore, object weight may alter the peak vibrational frequency of the MR system. As such, if the peak vibrational frequency of a system at a particular site is known, the pulse polarity scheme may be site dependent and tailored for the MR system vibrational frequency. Furthermore, if a particular pulse polarity scheme is determined to be more effective compared with other pulse polarity schemes in reducing artifacts and ghosting for the MR system, the particular pulse polarity scheme so determined may be used as a default pulse polarity scheme for all diffusion weighted scans performed on the given MR system. As such, process flow **105** may direct technique **90** to perform the diffusion weighted scan that incorporates the particular pulse polarity scheme **104** after determining the particular pulse polarity scheme **94**. Alternatively, the pulse polarity scheme may be site independent where a default, or predetermined, MR sys-

tem vibrational frequency is used. The default vibrational frequency may be found, for example, based on an average of known vibrational frequencies for a class of MR systems. Similarly, the pulse polarity scheme for a particular site may be made object dependent upon determining changes in the MR system peak vibrational frequency due to object weight on a per scan basis.

FIGS. **4-13** show exemplary pulse polarity schemes and corresponding SSE pulse sequence frequency spectra corresponding thereto according to aspects of the present invention. A series of polarity designators **106** is determined for a $2*TR$ interval. The $2*TR$ interval includes a TR_1 interval and a TR_2 interval. Each polarity designator **106** represents a polarity of a pair of diffusion gradient pulses, such as pulses **72**, **74** of FIG. **2**, for each slice of a multi-slice imaging scan. The polarity designator **106** represents the polarity of the pair of diffusion gradient pulses that will be applied during each slice of the multi-slice imaging scan. That is, the polarity of the pair of diffusion gradient pulses may be positive or negative. A blade of MR data for a multi-blade imaging scan is acquired in each TR interval. Initially, the polarity of each polarity designator in the pulse polarity scheme is set to a positive polarity or a negative polarity. Next, the polarity of each polarity designator may be inverted, or "chopped", to an opposite polarity according to an inversion sequence to form the pulse polarity scheme.

FIG. **4** shows a pulse polarity scheme **108** having the inversion sequence set to "None". That is, the "None" inversion sequence does not invert the polarity of any polarity designator **106**.

FIG. **5** shows a frequency spectrum **110** corresponding to a Fourier transform of the pulse polarity scheme **108** of FIG. **4** applied to SSE diffusion gradients. Frequency spectrum **110** shows calculated vibrational frequencies induced with an exemplary gradient coil assembly having diffusion gradient pulses according to the pulse polarity scheme **108** applied thereto. As shown, frequency spectrum **110** shows peak frequencies **111** offset from 10 Hz.

FIG. **6** shows a pulse polarity scheme **112** having the inversion sequence set to "Blade". In the "Blade" inversion sequence, the polarities of the polarity designators **106** in the first "M" blades are not inverted. Thereafter, the polarities of the polarity designators **106** in the next "M" blades are inverted. The inversion sequence is repeated such that every other group of "M" blades includes inverted polarity designators **106**. As shown in FIG. **6**, the polarity of the polarity designators **106** in one blade is not inverted, for example, in the TR_1 interval, while the polarity of the polarity designators **106** in the next TR are inverted. In this manner, "M" is set to 1. That is, the polarity of the polarity designators **106** in every other blade is inverted. As such, a multi-blade imaging scan according to pulse polarity scheme **112** includes application of diffusion gradient pulses for a first blade having a positive polarity and application of diffusion gradient pulses for a second blade having a negative polarity.

FIG. **7** shows a frequency spectrum **114** corresponding to a Fourier transform of the pulse polarity scheme **112** of FIG. **6** applied to SSE diffusion gradients. Frequency spectrum **114** shows calculated vibrational frequencies induced with an exemplary gradient coil assembly having SSE diffusion gradient pulses according to the pulse polarity scheme **112** applied thereto. Peak frequencies **115** non-coincident with 10 Hz are illustrated.

FIG. **8** shows a pulse polarity scheme **116** having the inversion sequence set to "Slice". In the "Slice" inversion sequence, the polarities of the first "N" polarity designators **106** are not inverted. Thereafter, the polarities of the next "N"

polarity designators **106** are inverted. The inversion sequence is repeated such that every other group of “N” slices in the blade is inverted. The “Slice” inversion sequence repeats the inversion sequence as described in the succeeding blade. As shown in FIG. **8**, “N” is set to 1. That is, the polarity of the polarity designator **106** of every other slice is inverted. Preferably, the value of “N” is an integer between zero and the total number of slices in the blade. Setting “N” equal to 0, for example, results in an inversion sequence identical to the “None” inversion sequence of FIG. **4**. Similarly, setting “N” equal to 18, for example, results in an inversion sequence identical to the “Blade” inversion sequence of FIG. **6**.

FIG. **9** shows a frequency spectrum **118** corresponding to a Fourier transform of the pulse polarity scheme **116** of FIG. **8** applied to SSE diffusion gradients. Frequency spectrum **118** shows calculated vibrational frequencies induced with an exemplary gradient coil assembly having SSE diffusion gradient pulses according to the pulse polarity scheme **116** applied thereto. Frequency spectrum **118** shows harmonic peaks **119** inconsistent with 10 Hz.

FIG. **10** shows a pulse polarity scheme **120** having the inversion sequence set to “Slice and Blade”. In the “Slice and Blade” inversion sequence, the polarities of the polarity designators **106** are set according to the “Slice” inversion sequence as previously described. Then, the polarities of the polarity designators **106** in one of the blades are inverted.

FIG. **11** shows a frequency spectrum **122** corresponding to a Fourier transform of the pulse polarity scheme **120** of FIG. **10** applied to SSE diffusion gradients. Frequency spectrum **122** shows calculated vibrational frequencies induced with an exemplary gradient coil assembly having SSE diffusion gradient pulses according to the pulse polarity scheme **120** applied thereto. Frequency spectrum **122** shows harmonic peaks **123** offset from 10 Hz.

FIG. **12** shows a pulse polarity scheme **124** having the inversion sequence set to “Random”. In the “Random” inversion sequence, the polarities of the polarity designators **106** are randomly inverted. In this manner, the polarities of the polarity designators **106** are not inverted according to a prescribed pattern. Rather, the polarity of each polarity designator **106** is randomly inverted. The “Random” inversion sequence may randomly invert the polarity designators **106** over the 2^*TR interval as shown, or alternatively, the polarity designators **106** may be randomly inverted over an N^*TR interval where the “Random” inversion sequence repeats as often as every N TR intervals or where the “Random” inversion sequence never repeats for an entire scan.

FIG. **13** shows a frequency spectrum **126** corresponding to a Fourier transform of the pulse polarity scheme **124** of FIG. **12** applied to SSE diffusion gradients. Frequency spectrum **126** shows calculated vibrational frequencies induced with an exemplary gradient coil assembly having SSE diffusion gradient pulses according to the pulse polarity scheme **124** applied thereto. The calculated vibrational frequencies illustrate diminishing vibrational frequency peaks **127** from 0 Hz to 20 Hz.

The terms “None”, “Blade”, “Slice”, “Slice and Blade”, and “Random” of the pulse polarity schemes **108**, **112**, **116**, **120**, **124** above are exemplary terms that are intended to refer to the pulse polarity scheme labeled thereby for identification and are not intended to limit the pulse polarity schemes **108**, **112**, **116**, **120**, **124** to a particular form. As such, it is contemplated that other or additional nomenclature may be used to distinguish between various pulse polarity schemes.

In addition to inverting the polarities of diffusion weighted pulses between blades or slices, the shape of the diffusion weighted pulses may be modified to include an inversion

thereof. FIG. **14** shows a pulse sequence to acquire Dual Spin Echo (DSE) diffusion weighted MR images according to another embodiment of the present invention. Pulses **72**, **74** of FIG. **2** may each be modified from a single pulse to a series of multiple pulses. As shown in FIG. **14**, pulses **72**, **74** are each modified in a diffusion gradient sequence **140** to include a pair of alternating polarity diffusion gradient pulses **142**, **144** and **146**, **148**, respectively. It is contemplated, however, that pulses **72**, **74** may each be modified to include more than two pulses. In a preferred embodiment, pulses **142**, **144** are applied before and after a slice selective pulse **150**, respectively, and pulses **146**, **148** are applied before and after a slice selective pulse **152**, respectively. As shown, diffusion gradient pulses **142**, **144**, **146**, **148** are applied along an x axis for each image slice; however, it is contemplated that diffusion gradient pulses **142**, **144**, **146**, **148** may be similarly applied along other axes, such as a y axis or a z axis. A gradient area sum of pulse areas **154**, **156**, **158**, **160** is preferably substantially equal to zero to reduce low frequency vibrational content.

A ratio of widths of pulse **142** to pulse **144** may be varied to produce a desired frequency harmonic distribution. In a preferred embodiment, the ratio is varied between 0.0 and 1.0; however, it is contemplated that the ratio may be varied greater than 1.0. TE is reduced as the ratio changes from 0.0 to 0.5, and TE is increased as the ratio changes from 0.5 to 1.0. As TE becomes shorter, the signal-to-noise ratio (SNR) of the acquired data increases. Conversely, as TE becomes longer, the SNR of the acquired data decreases. Additionally, a height and shape of pulses **142**, **144**, **146**, **148** may be independently modified to further tailor MR system vibration frequencies caused thereby. For example, the shape of pulses **142**, **144**, **146**, **148** may be modified to a sinusoidal-type shape.

The polarities of pulses **142**, **144**, **146**, **148** alternate between pulses. That is, the polarities of pulses **142**, **146** are opposite that of pulses **144**, **148**. The pulse polarity schemes **108**, **112**, **116**, **120**, **124** may be applied to the DSE diffusion weighted pulses **142**, **144**, **146**, **148** between slices and/or blades according to the invention as described above. However, the polarity of the polarity designators **106** corresponds to the polarity of pulses **142**, **146** of diffusion gradient sequence **140**, and the polarity of pulses **144**, **148** is opposite that of pulses **142**, **146**. That is, if the polarity of the polarity marker **106** is positive, then the polarities of pulses **142**, **144**, **146**, **148** are set to positive, negative, positive, and negative, respectively. If the polarity of the polarity marker **106** is negative, then the polarities of pulses **142**, **144**, **146**, **148** are set to negative, positive, negative, and positive, respectively.

FIG. **15** shows a frequency spectrum **162** corresponding to a Fourier transform of the pulse polarity scheme **108** of FIG. **4** applied to DSE diffusion gradients. Frequency spectrum **162** shows calculated vibrational frequencies induced with an exemplary gradient coil assembly having DSE diffusion gradient pulses according to the pulse polarity scheme **108** applied thereto. As shown, frequency spectrum **162** shows peak frequencies **164** offset from 10 Hz.

FIG. **16** shows a frequency spectrum **166** corresponding to a Fourier transform of the pulse polarity scheme **112** of FIG. **6** applied to DSE diffusion gradients. Frequency spectrum **166** shows calculated vibrational frequencies induced with an exemplary gradient coil assembly having DSE diffusion gradient pulses according to the pulse polarity scheme **112** applied thereto. Frequency spectrum **166** shows harmonic peaks **168** inconsistent with 10 Hz.

FIG. **17** shows a frequency spectrum **170** corresponding to a Fourier transform of the pulse polarity scheme **116** of FIG. **8** applied to DSE diffusion gradients. Frequency spectrum

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170 shows calculated vibrational frequencies induced with an exemplary gradient coil assembly having DSE diffusion gradient pulses according to the pulse polarity scheme 116 applied thereto. Peak frequencies 172 non-coincident with 10 Hz are illustrated.

FIG. 18 shows a frequency spectrum 174 corresponding to a Fourier transform of the pulse polarity scheme 120 of FIG. 10 applied to DSE diffusion gradients. Frequency spectrum 174 shows calculated vibrational frequencies induced with an exemplary gradient coil assembly having DSE diffusion gradient pulses according to the pulse polarity scheme 120 applied thereto. Frequency spectrum 174 shows harmonic peaks 176 offset from 10 Hz.

FIG. 19 shows a frequency spectrum 178 corresponding to a Fourier transform of the pulse polarity scheme 124 of FIG. 12 applied to DSE diffusion gradients. Frequency spectrum 178 shows calculated vibrational frequencies induced with an exemplary gradient coil assembly having DSE diffusion gradient pulses according to the pulse polarity scheme 124 applied thereto. The calculated vibrational frequencies illustrate increasing 174 vibrational frequency peaks 180 from 0 Hz to 20 Hz.

FIG. 20 shows another technique for reducing vibration-related artifacts according to the present invention. Technique 182 begins at step 184 by determining a mechanical vibrational frequency of an MR system prior to performing a scan. Next, a plurality of parameters is determined 186 that affects the mechanical resonant frequency of the MR system. The parameters may include the number of slices, the duration of TR, and echo train length (ETL); however, the parameters are not so limited. At step 188, the parameters are varied, and vibrational frequencies induced on the MR system for each parameter variation are calculated. A range of the parameters is determined that induces vibrational frequencies coincident with the vibrational frequency of the MR system at step 190. Parameters outside the range are then used to guide prescription of a diffusion weighted scan at step 192.

FIG. 21 shows a DW-PROPELLER image reconstructed from MR data acquired with a known diffusion weighted imaging technique. The MR data was acquired with SSE diffusion gradients applied along the right-left direction. As shown, the image has significant ghosting and artifacts.

FIG. 22 shows a DW-PROPELLER image reconstructed from MR data acquired using a technique according to the present invention. SSE diffusion gradients were applied along the right-left direction according to the "Blade and Slice" polarity scheme as described above. As shown, the reconstructed image shows reduced motion artifacts and ghosting compared with the image of FIG. 15.

The exemplary frequency spectra 110, 114, 118, 122, 126 may be used to determine a particular frequency spectrum having a vibrational frequency least coincident with an MR system vibrational frequency relative to the remaining frequency spectra. However, other factors related to the MR system, the gradient coil, and/or the diffusion weighted scan parameters may influence the selection of the desired pulse polarity scheme to be used in a given diffusion weighted MR scan. As such, the frequency spectrum having a vibrational frequency least coincident with an MR system vibrational frequency relative to the remaining frequency spectra may not be desirable for the diffusion weighted MR scan. In this regard, it is contemplated that the diffusion weighted scan may utilize a pulse polarity scheme of reduced vibrational frequency coincidence, but not necessarily the polarity scheme with the least coincidence.

Therefore, in accordance with one embodiment of the invention, an MR apparatus includes an MR system having a

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plurality of gradient coils positioned about a bore of a magnet to impress a polarizing magnetic field. An RF transceiver system and an RF switch are controlled by a pulse module to transmit and receive RF signals to and from an RF coil assembly to acquire MR images. The MR apparatus also includes a computer programmed to determine a mechanical resonant frequency of the MR system and acquire diffusion weighted MR data such that vibration harmonics generated during application of diffusion weighted gradients to acquire the diffusion weighted MR data do not coincide with the mechanical resonant frequency of the MR system.

In accordance with another embodiment, a method of MR imaging includes the step of determining a plurality of diffusion gradient pulse sequences, each diffusion gradient pulse sequence having a plurality of diffusion weighted gradient pulses. The method also includes the steps of modeling each of the plurality of diffusion gradient pulse sequences with a distinct gradient amplitude and polarity versus time function having a polarity marker for the plurality of diffusion weighted gradient pulses and generating a temporal frequency spectrum of vibrational forces induced with each of the modeled plurality of diffusion gradient pulse sequences. The method further includes selecting a modeled diffusion gradient pulse sequence from the plurality of modeled diffusion gradient pulse sequences having a temporal frequency spectrum dissimilar from a mechanical resonance frequency spectrum of an MR system and applying the selected modeled diffusion gradient pulse sequence in an MR scan.

In accordance with another embodiment of the invention, the invention is embodied in a computer program stored on a computer readable storage medium and having instructions which, when executed by a computer, cause the computer to determine a mechanical resonant vibration frequency of an MR apparatus and determine a series of diffusion gradient pulse polarity schemes for diffusion weighted gradients to be applied by gradient coils of the MR apparatus. A frequency spectrum is calculated of vibrational forces induced for each of the diffusion gradient pulse polarity schemes. The instructions further cause the computer to identify a frequency spectrum having at least one spectral peak at a frequency inconsistent with the mechanical vibration frequency of the MR apparatus and perform a diffusion weighted MR scan of an imaging subject with application of diffusion weighted gradients being governed by the diffusion gradient pulse polarity scheme corresponding to the identified frequency spectrum.

In accordance with yet another embodiment of the invention, a method of MR imaging includes the steps of measuring a mechanical resonant frequency of an MR scanner and determining a range of parameters whose corresponding pulse sequence has a gradient sequence that excites the mechanical resonant frequencies of the MR scanner during an MR scan. The use of the MR scanner is limited based on the determined range of parameters.

The present invention has been described in terms of the preferred embodiment, and it is recognized that equivalents, alternatives, and modifications, aside from those expressly stated, are possible and within the scope of the appending claims.

What is claimed is:

1. A method of magnetic resonance (MR) imaging comprising the steps of:
 - generating a temporal frequency spectrum of vibrational forces induced with a diffusion gradient pulse sequence having a plurality of diffusion weighted gradient pulses;

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applying the diffusion gradient pulse sequence in an MR scan if the generated temporal frequency spectrum is dissimilar from a mechanical resonance frequency spectrum of an MR system.

2. The method of claim 1 further comprising the step of modeling diffusion gradient pulse sequence with a gradient amplitude and polarity versus time function having a polarity marker for the plurality of diffusion weighted gradient pulses.

3. The method of claim 1 further comprising the step of assuming the mechanical resonance frequency spectrum of the MR system to be generic for a class of MR systems to which the MR system belongs.

4. The method of claim 1 further comprising the step of determining the mechanical resonance frequency spectrum from vibrational data collected with an accelerometer.

5. The method of claim 1 wherein the plurality of diffusion weighted gradient pulses includes Dual Spin Echo diffusion weighted gradient pulses.

6. The method of claim 2 wherein the step of modeling comprises modeling each of the plurality of diffusion gradient pulse sequences over a $2*TR$ interval, the $2*TR$ interval comprising a TR_1 interval followed by a TR_2 interval.

7. The method of claim 6 further comprising the step of determining the gradient amplitude and polarity versus time function by:

setting the polarity of a first polarity marker in the TR_1 interval equal to one of a positive polarity and a negative polarity;

setting polarities of the remaining polarity markers in the TR_1 interval equal to the polarity of the first polarity marker; and

setting polarities of the polarity markers in the TR_2 interval equal to a polarity equal to that of the polarity markers in the TR_1 interval.

8. The method of claim 6 further comprising the step of determining the gradient amplitude and polarity versus time function by:

setting the polarity of a first polarity marker in each of a first set of M TR intervals equal to one of a positive polarity and a negative polarity;

setting polarities of the remaining polarity markers in the first set of M TR intervals equal to the polarity of the first polarity marker;

setting polarities of the polarity markers in a second set of M TR intervals equal to a polarity opposite that of the polarity markers in the first set of M TR intervals; and

wherein M is an integer greater than zero.

9. The method of claim 6 further comprising the step of determining the gradient amplitude and polarity versus time function by:

setting the polarity of a first set of N polarity markers in the TR_1 interval equal to one of a positive polarity and a negative polarity;

setting the polarity of each succeeding set of N polarity markers in the TR_1 interval equal to a polarity opposite that of the preceding set of N polarity markers;

setting the polarity of a first set of N polarity markers in the TR_2 interval equal to the polarity of the first set of N polarity markers in the TR_1 interval;

setting the polarity of each succeeding set of N polarity markers in the TR_2 interval equal to a polarity opposite that of the preceding set of N polarity markers; and

wherein N is an integer greater than zero.

10. The method of claim 6 further comprising the step of determining the gradient amplitude and polarity versus time function by:

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setting the polarity of a first set of N polarity markers in the TR_1 interval equal to one of a positive polarity and a negative polarity;

setting the polarity of each succeeding set of N polarity markers in the TR_1 interval equal to a polarity opposite that of the preceding set of N polarity markers;

setting the polarity of a first set of N polarity markers in the TR_2 interval equal to a polarity opposite that of the first set of N polarity markers in the TR_1 interval;

setting the polarity of each succeeding set of N polarity markers in the TR_2 interval equal to a polarity opposite that of the preceding set of N polarity markers; and

wherein N is an integer greater than zero.

11. The method of claim 6 further comprising the step of determining the gradient amplitude and polarity versus time function by randomly setting the polarity of each polarity marker in the $2*TR$ interval equal to one of a positive polarity and a negative polarity.

12. The method of claim 2 further comprising the steps of: determining a vibration frequency spectrum of the MR system;

identifying harmonic peaks in the vibration frequency spectrum of the MR system;

identifying harmonic peaks in the temporal frequency spectrum; and

determining a similarity of harmonic peaks between the temporal frequency spectrum and the vibrational frequency spectrum of the MR system.

13. The method of claim 1 wherein the step of applying the diffusion gradient pulse sequence comprises applying the diffusion gradient pulse sequence in one of a diffusion weighted periodically rotated overlapping parallel line with enhanced reconstruction (DW-PROPELLER) scan and a diffusion weighted echo planar imaging (DWEPI) scan.

14. A computer readable storage medium having a computer program stored thereon and representing a set of instructions that when executed by a computer causes the computer to:

calculate a frequency spectrum of vibrational forces induced with a diffusion gradient pulse polarity scheme;

perform a diffusion weighted magnetic resonance (MR) scan of an imaging subject with application of diffusion weighted gradients being governed by the diffusion gradient pulse polarity scheme if the frequency spectrum has at least one spectral peak at a frequency inconsistent with a mechanical vibration frequency of an MR apparatus.

15. The computer readable storage medium of claim 14 wherein the set of instructions further causes the computer to determine the diffusion gradient pulse polarity scheme for a specific MR apparatus after the MR apparatus has been delivered to a site location.

16. The computer readable storage medium of claim 14 wherein the set of instructions further causes the computer to determine the diffusion gradient pulse polarity scheme on a per-patient basis.

17. The computer readable storage medium of claim 14 wherein the set of instructions further causes the computer to perform the diffusion weighted MR scan with application of Dual Spin Echo diffusion weighted gradients.

18. The computer readable storage medium of claim 14 wherein the set of instructions further causes the computer to determine the diffusion gradient pulse polarity scheme by determining a single-polarity diffusion gradient pulse polarity scheme.

19. The computer readable storage medium of claim 14 wherein the set of instructions further causes the computer to

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determine the diffusion gradient pulse polarity scheme by determining at least one dual-polarity diffusion gradient pulse polarity scheme.

20. The computer readable storage medium of claim 19 wherein the set of instructions further causes the computer to determine the at least one dual-polarity diffusion gradient pulse of the diffusion gradient pulse polarity scheme equal to one of a positive polarity and a negative polarity according to one of an every M blades polarity scheme, an every N slices polarity scheme, an every other slice and blade polarity

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scheme, and a random polarity scheme, where M is an integer representing a number of inverted blades in a blade inversion group and where N is an integer representing a number of inverted slices in a slice inversion group.

21. The computer readable storage medium of claim 14 wherein the set of instructions further causes the computer to determine the mechanical vibration frequency of the MR apparatus from a presumed mechanical vibration frequency value for the MR apparatus.

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