



US006897655B2

(12) **United States Patent**  
**Brittain et al.**

(10) **Patent No.:** **US 6,897,655 B2**  
(45) **Date of Patent:** **May 24, 2005**

(54) **MOVING TABLE MRI WITH  
FREQUENCY-ENCODING IN THE  
Z-DIRECTION**

(75) Inventors: **Jean H. Brittain**, Palo Alto, CA (US);  
**John M. Pauly**, Redwood City, CA  
(US)

(73) Assignees: **General Electric Company**,  
Milwaukee, WI (US); **The Board of  
Trustees of the Leland Stanford, Jr.  
University**, Stanford, CA (US)

(\*) Notice: Subject to any disclaimer, the term of this  
patent is extended or adjusted under 35  
U.S.C. 154(b) by 0 days.

(21) Appl. No.: **10/235,454**

(22) Filed: **Sep. 4, 2002**

(65) **Prior Publication Data**

US 2003/0011369 A1 Jan. 16, 2003

**Related U.S. Application Data**

(63) Continuation of application No. 09/682,699, filed on Oct. 5,  
2001, which is a continuation-in-part of application No.  
09/681,420, filed on Mar. 30, 2001.

(51) **Int. Cl.**<sup>7</sup> ..... **G01V 3/00**; A61B 5/05

(52) **U.S. Cl.** ..... **324/309**; 600/410; 600/415;  
324/318; 324/307; 324/306

(58) **Field of Search** ..... 600/410, 420,  
600/407-423; 324/309, 318, 307, 300-322

(56) **References Cited**

**U.S. PATENT DOCUMENTS**

5,928,148	A	7/1999	Wang et al.	
6,385,478	B1 *	5/2002	Hajnal	600/410
6,584,337	B2 *	6/2003	Dumoulin et al.	600/410
6,617,850	B2 *	9/2003	Welch et al.	324/309
2002/0173715	A1 *	11/2002	Kruger et al.	600/410
2003/0100825	A1 *	5/2003	Demoulin et al.	600/410

**FOREIGN PATENT DOCUMENTS**

JP	H06304153	1/1994
JP	H06311977	8/1994
JP	H08173396	9/1996

**OTHER PUBLICATIONS**

U.S. Provisional Application No. 60/282,555, filed Apr. 9,  
2001, the Kruger et al.\*

U.S. Provisional Application No. 60/252,555, filed Apr. 9,  
2001, the Kruger et al.\*

K Liu, B. Rutt, "Sliding Interleaved ky (SLINKY) Acqui-  
sition: A Novel 3D MRA Technique with Suppressed Slab  
Boundary Artifact", JMRI, 8:903-911 (1998).

K Liu, D. Lee, B. Rutt, "Systematic Assessment and Evalu-  
ation of Sliding Interleaved ky (SLINKY) Acquisition for  
3D MRA", JMRI, 8:912-923 (1998).

(Continued)

*Primary Examiner*—G. Bradley Bennett

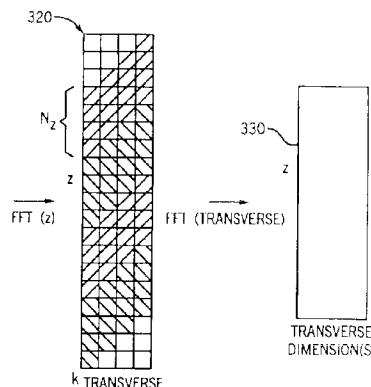
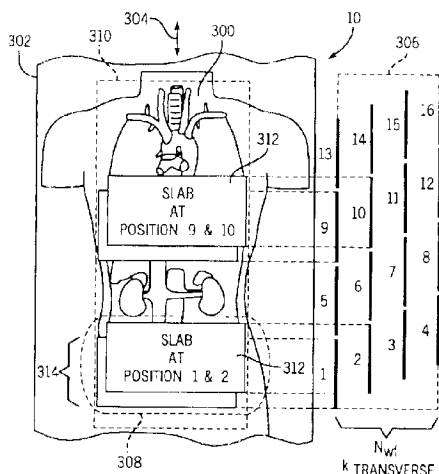
*Assistant Examiner*—Tiffany A. Fetzner

(74) *Attorney, Agent, or Firm*—Ziolkowski Patent  
Solutions Group, LLC; Michael A. Della Penna; Carl B.  
Horton

(57) **ABSTRACT**

A system and method are disclosed using continuous table  
motion while acquiring data to reconstruct MR images  
across a large FOV without significant slab-boundary arti-  
facts that reduces acquisition time. At each table position,  
full z-encoding data are acquired for a subset of the trans-  
verse k-space data. The table is moved through a number of  
positions over the desired FOV and MR data are acquired  
over the plurality of table positions. Since full z-data are  
acquired for each slab, the data can be Fourier transformed  
in z, interpolated, sorted, and aligned to match anatomic z  
locations. The fully sampled and aligned data is then Fourier  
transformed in remaining dimension(s) to reconstruct the  
final image that is free of slab-boundary artifacts.

**41 Claims, 10 Drawing Sheets**



OTHER PUBLICATIONS

K Liu, "SLINKY: More Understanding, Optimization and Application for High Resolution MRA", ISMRM Seventh Scientific Meeting, 1908, 1999.

K Liu, Y. Xu, M. Loncar, "Artifact Transformation Technique: Shifted Interleaved Multi-Volume Acquisition (SIMVA) for 3D FSE", ISMRM Sixth Scientific Meeting, 572, 1998.

K Liu, Y. Xu, M. Loncar, "Applications of Shifted-Interleaved Multi-Volume Acquisition (SIMVA) with Suppressed Slab Boundary Artifact", ISMRM Seventh Scientific Meeting, 1618, 1999.

J. Hennig, "Overlapping Section Coverage in Multisection Imaging", JMRI, 3:425-432 (1993).

J. Pipe, "Spatial Encoding and Reconstruction in MRI with Quadratic Phase Profiles", MRM, 33:24-33 (1995).

J. Pipe, "Analysis of Localized Quadratic Encoding and Reconstruction", MRM, 36: 137-146 (1996).

O'Dietrich, J. Hajnal, "Extending the Coverage of True Volume Scans by Continuous Movement of the Subject", ISMRM Seventh Scientific Meeting, 1653, 1999.

K Y. Ho, T. Leiner, M.H. de haan, J.M.A. van Engelshoven, "Gadolinium Optimized Tracking Technique: A new MRA technique for Imaging the Peripheral Vascular Tree from Aorta to the Foot using one Bolus of Gadolinium", ISMRM Fifth Scientific Meeting, 203, 1997.

\* cited by examiner

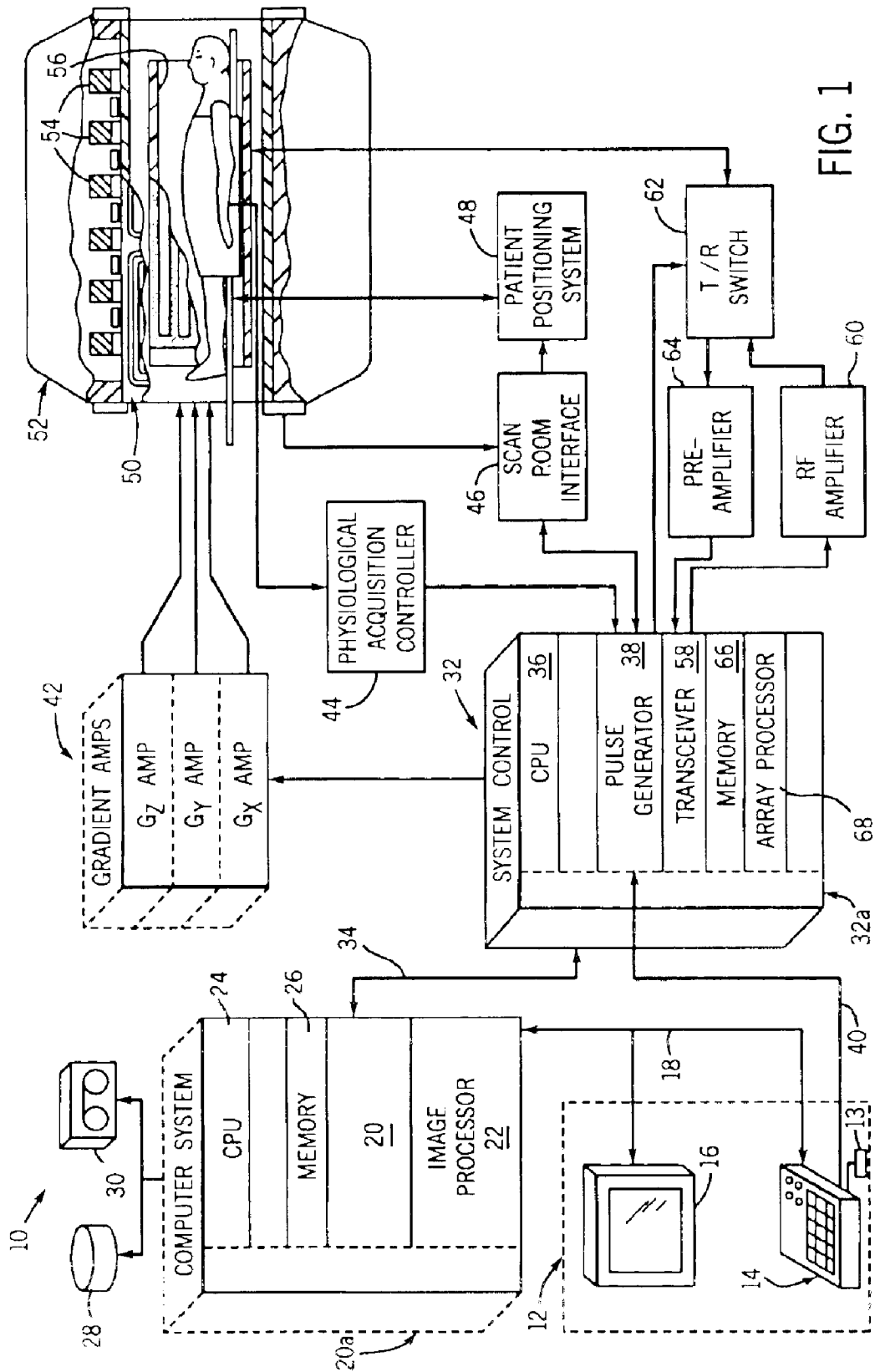


FIG. 1

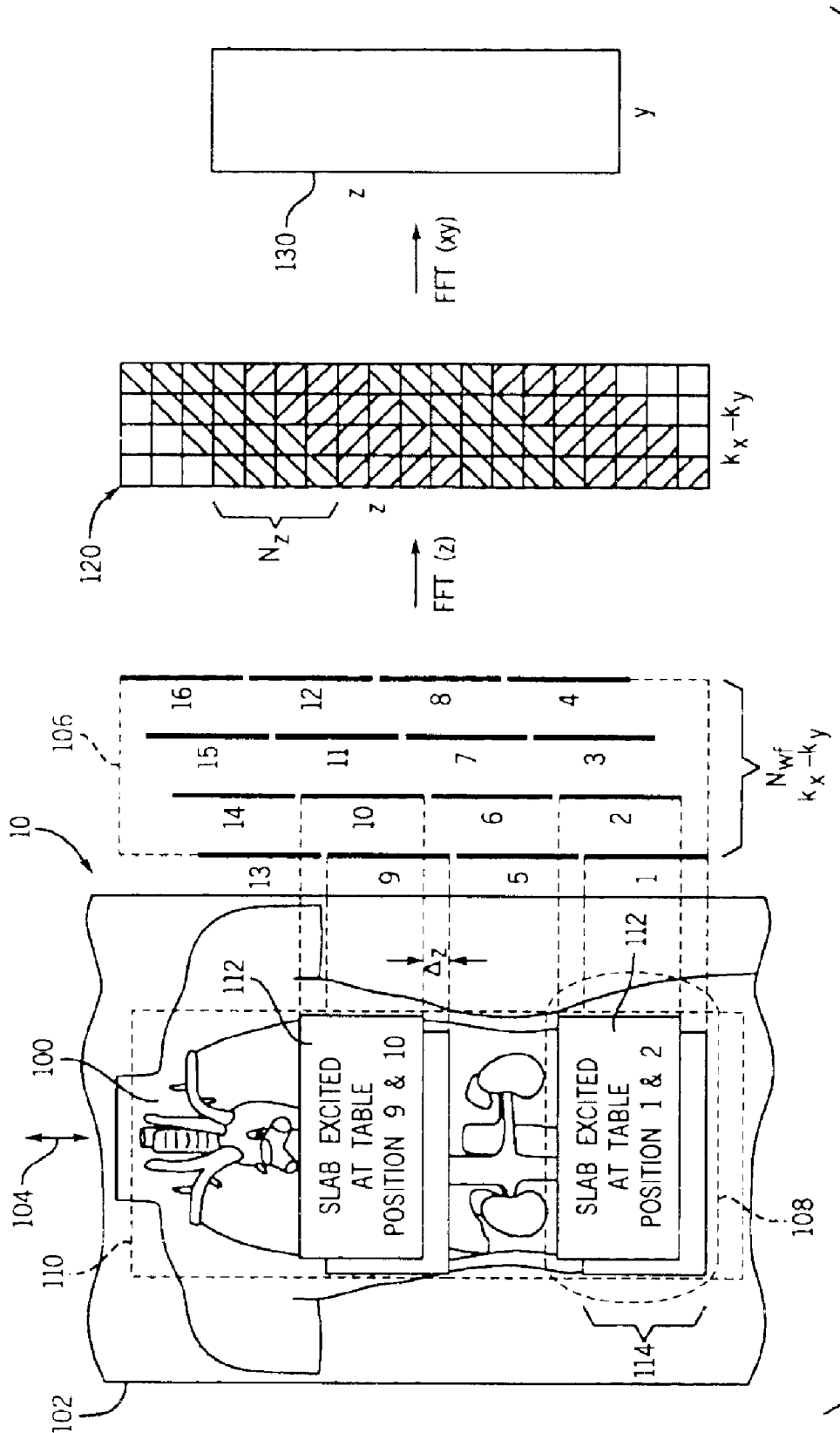


FIG. 2

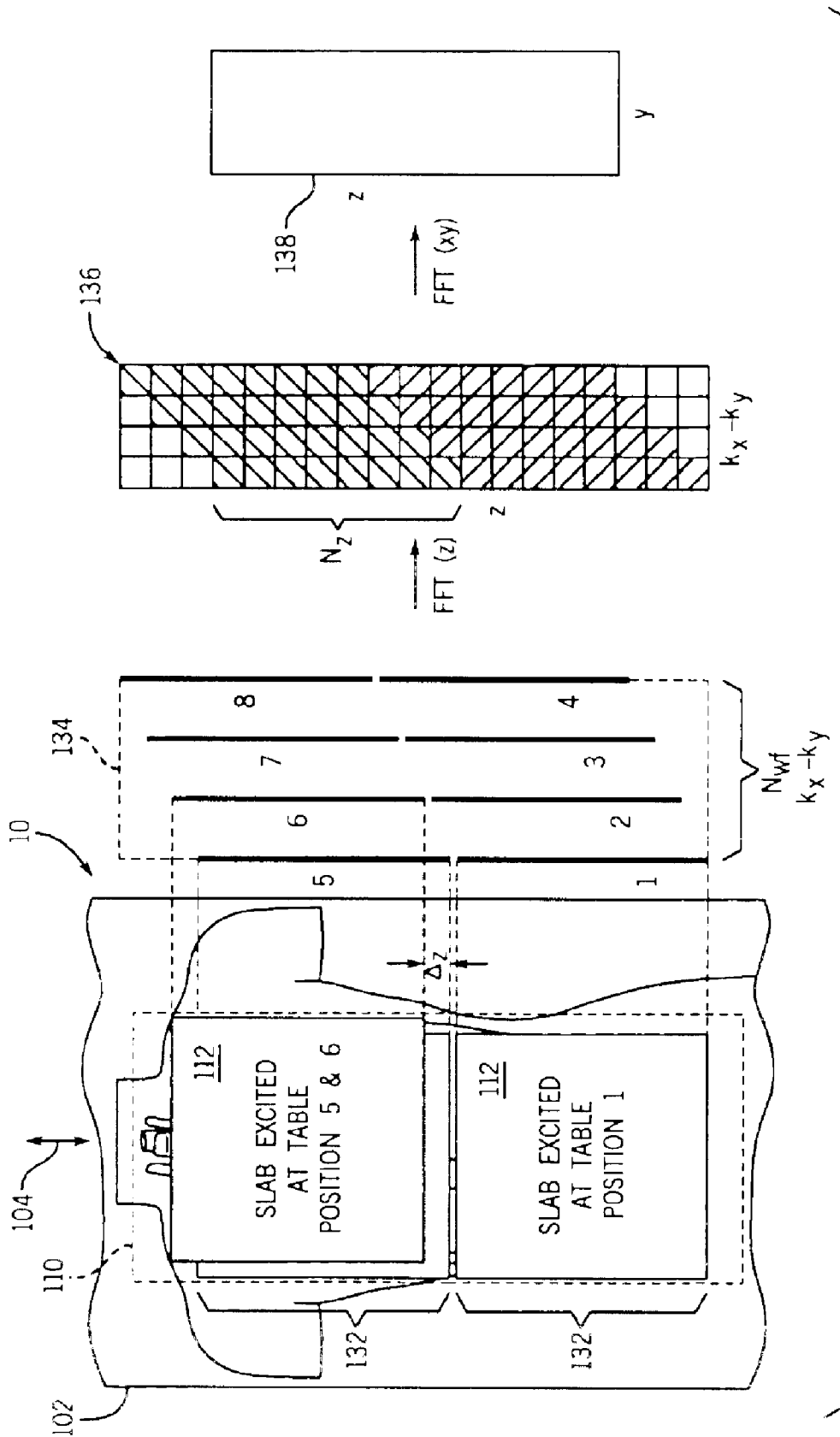


FIG. 3

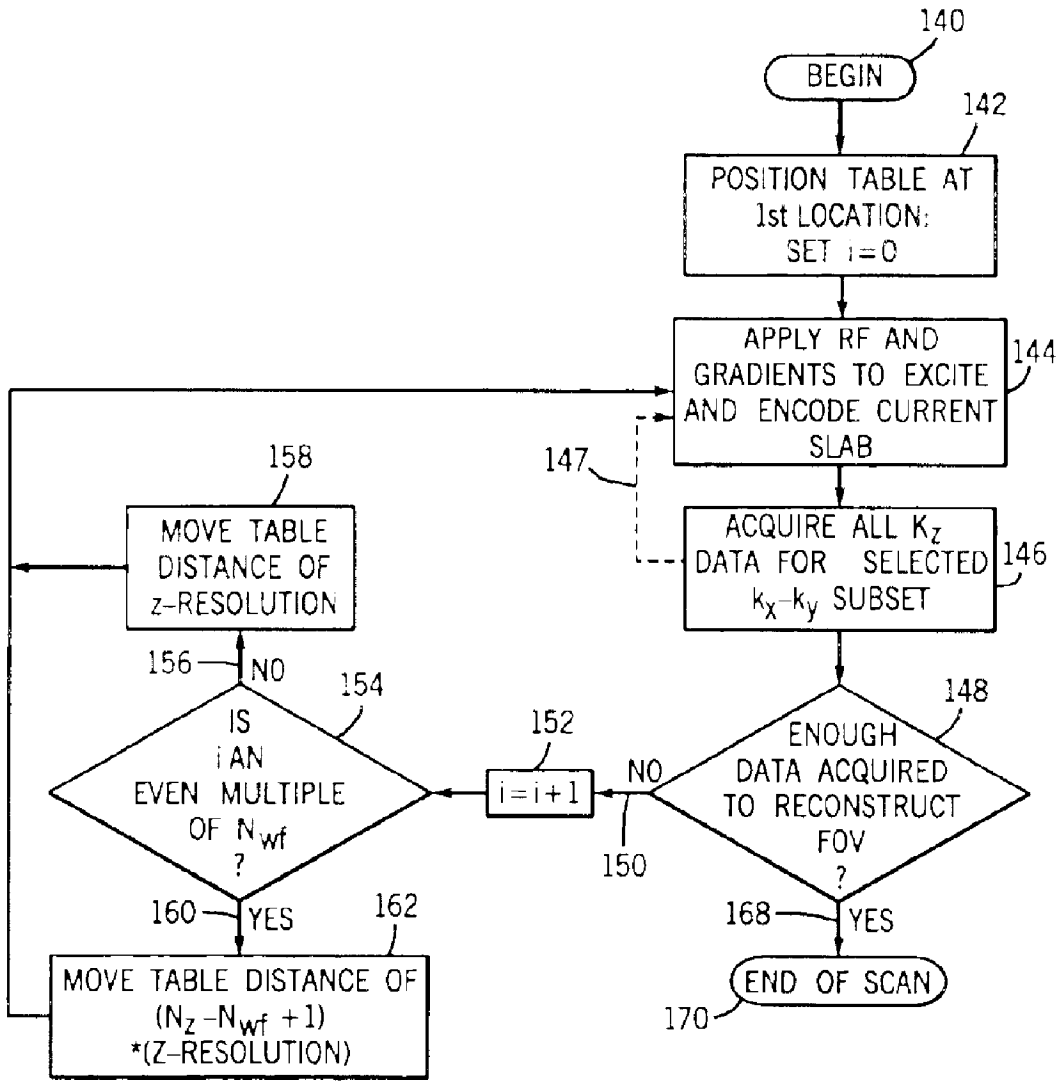


FIG. 4

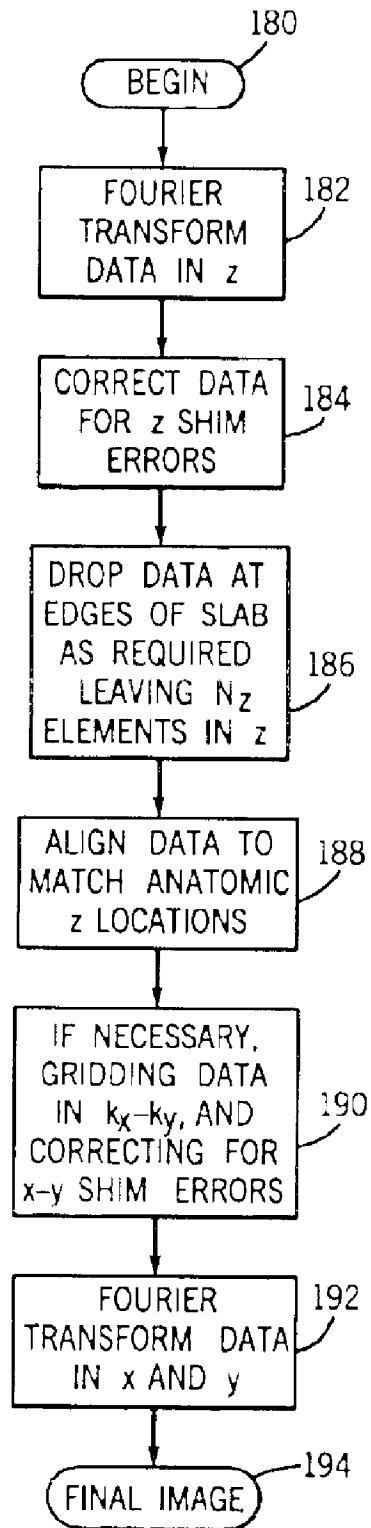
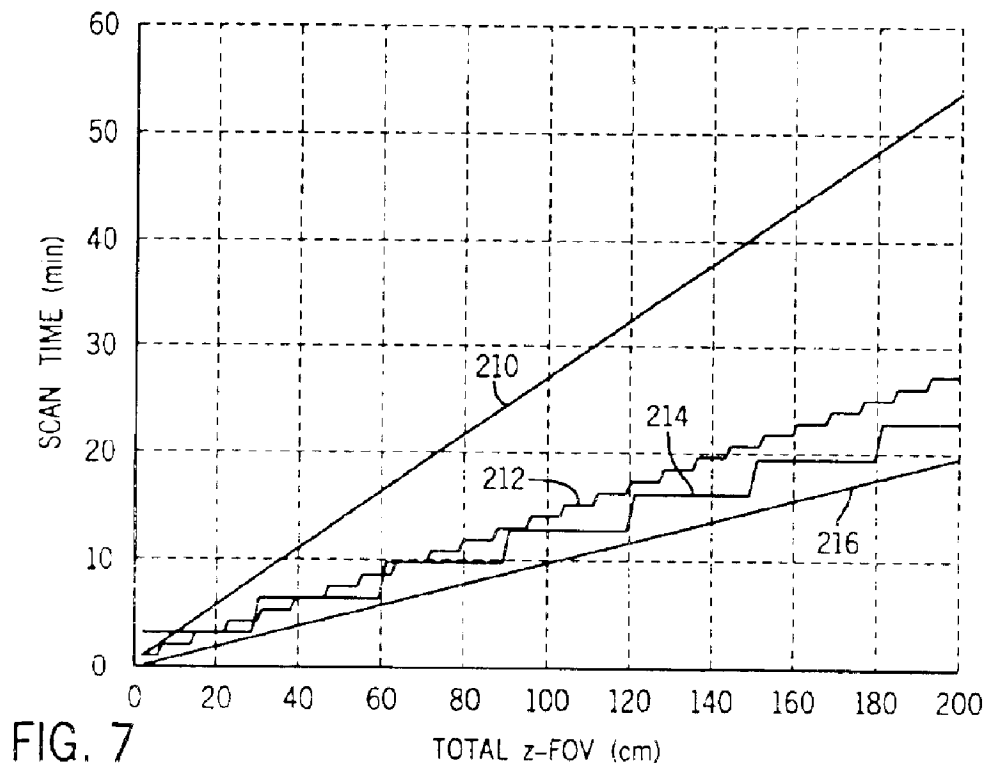
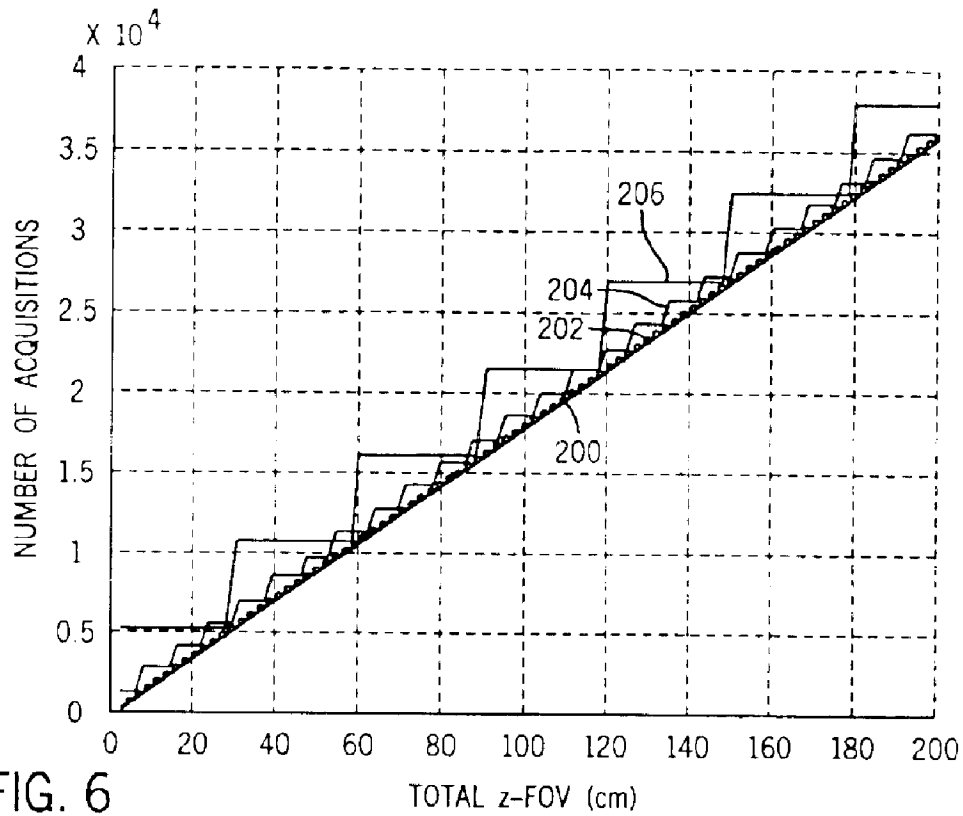


FIG. 5





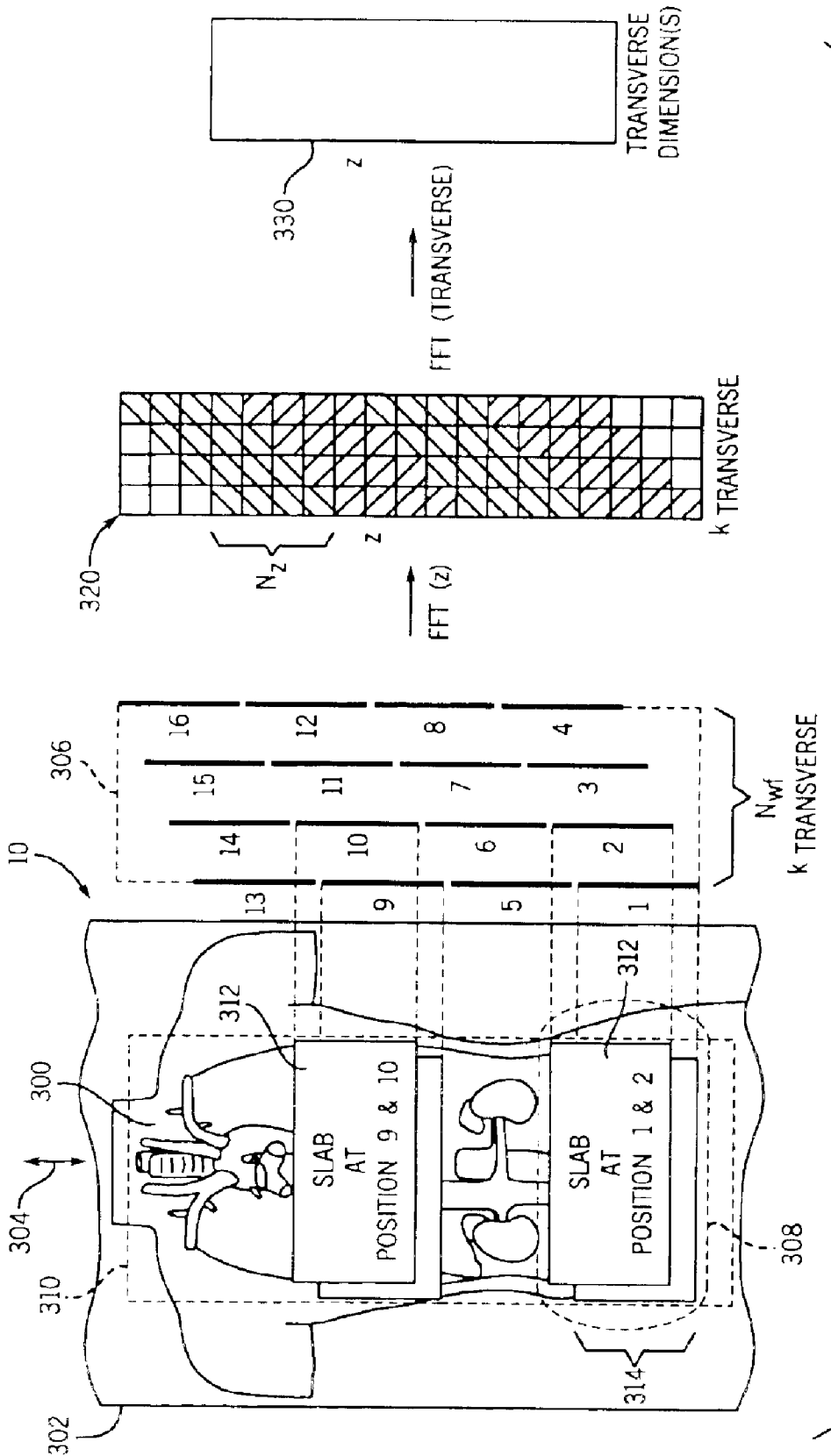


FIG. 8

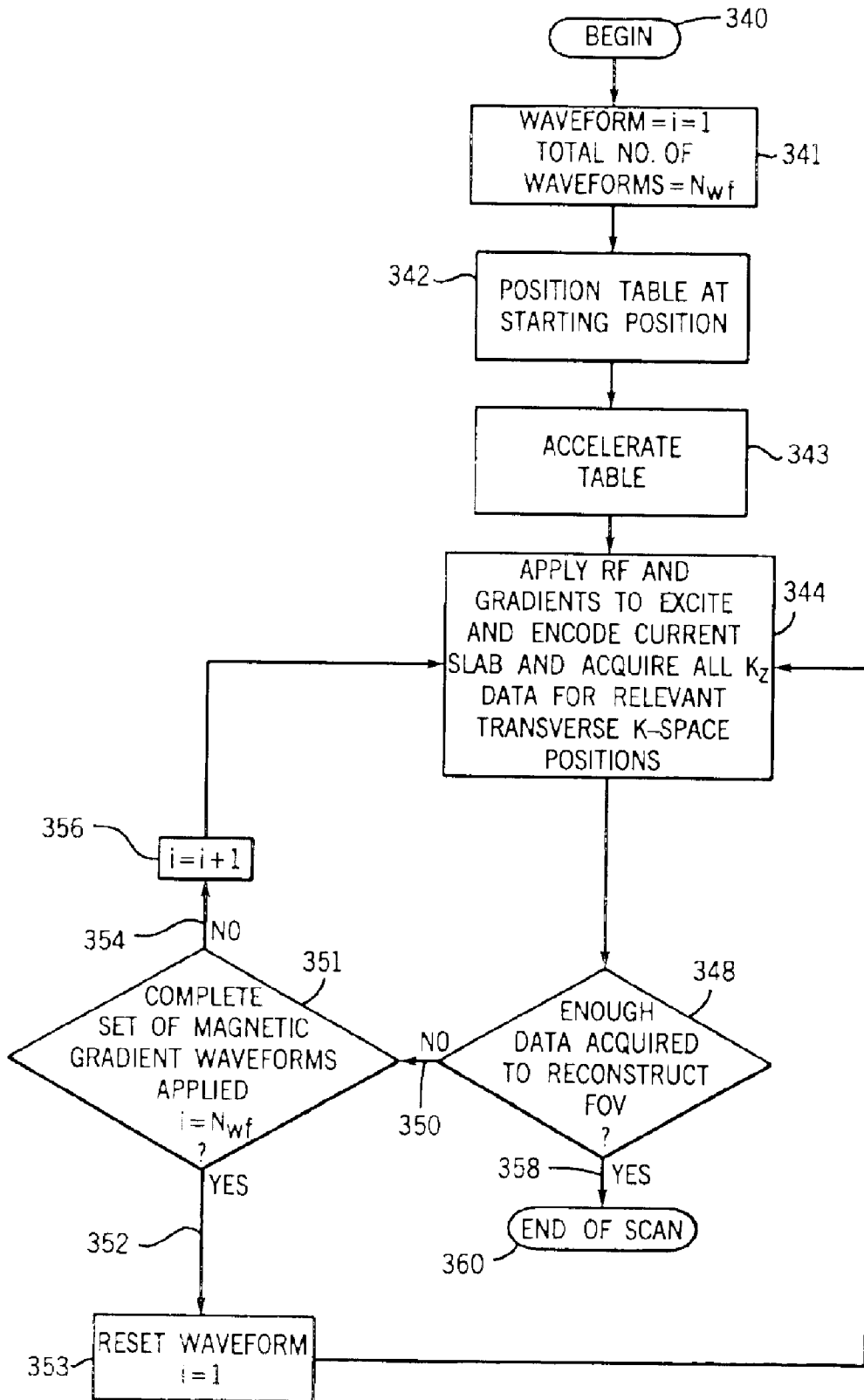


FIG. 9

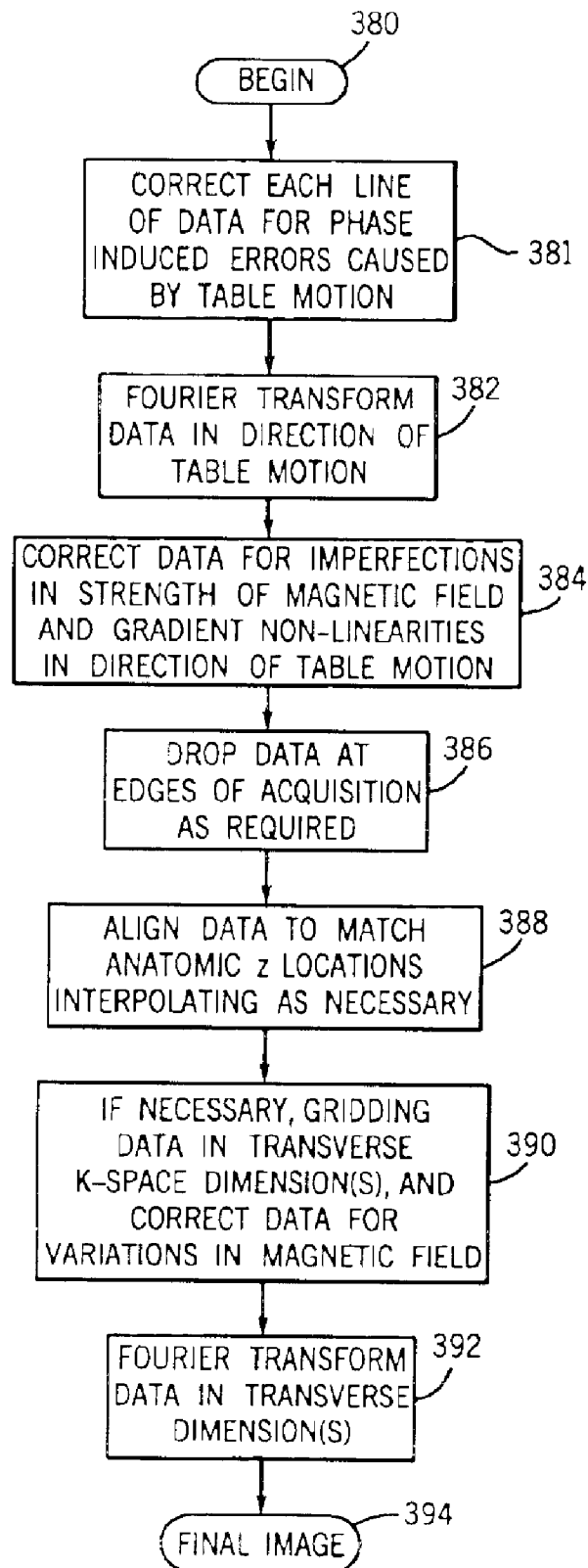
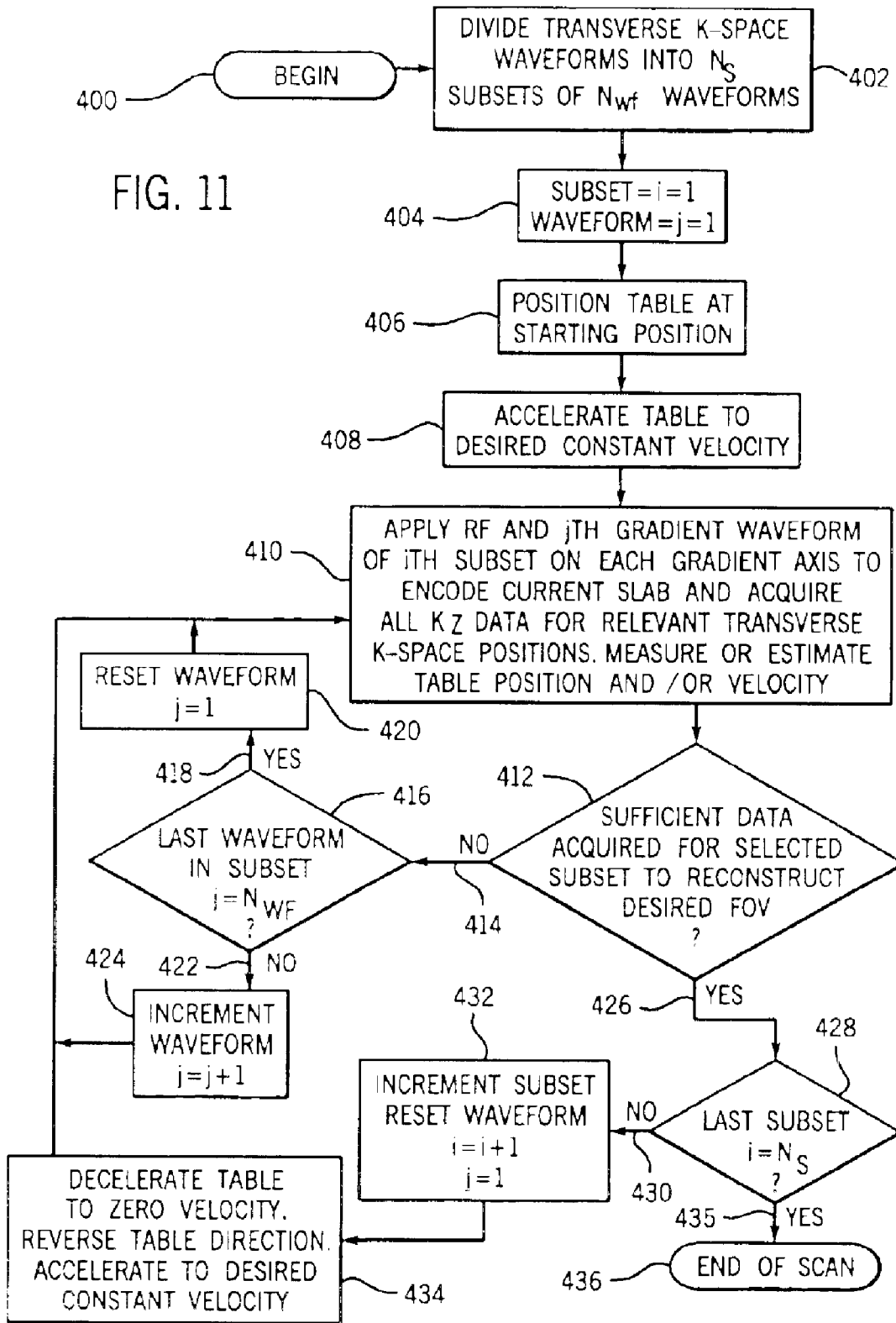


FIG. 10

FIG. 11



## MOVING TABLE MRI WITH FREQUENCY-ENCODING IN THE Z-DIRECTION

### CROSS-REFERENCE TO RELATED APPLICATIONS

This application is a continuation and claims priority of U.S. patent application Ser. No. 09/682,699 filed Oct. 5, 2001 which is a continuation-in-part and claims the priority of U.S. patent application Ser. No. 09/681,420 filed Mar. 30, 2001 entitled "Method And Apparatus of Acquiring Large FOV Images Without Slab-Boundary Artifacts".

### BACKGROUND OF THE INVENTION

The present invention relates generally to an improved method of medical imaging over large areas, and more particularly, to a method and apparatus of acquiring magnetic resonance (MR) images over an area that is greater than the optimal imaging area of an MR scanner using continuous table movement through the MR scanner without incurring slab-boundary artifacts.

When a substance such as human tissue is subjected to a uniform magnetic field (polarizing field  $B_0$ ), the individual magnetic moments of the spins in the tissue attempt to align with this polarizing field, but precess about it in random order at their characteristic Larmor frequency. If the substance, or tissue, is subjected to a magnetic field (excitation field  $B_1$ ) which is in the x-y plane and which is near the Larmor frequency, the net aligned moment, or "longitudinal magnetization",  $M_z$ , may be rotated, or "tipped", into the x-y plane to produce a net transverse magnetic moment  $M_r$ . A signal is emitted by the excited spins after the excitation signal  $B_1$  is terminated and this signal may be received and processed to form an image.

When utilizing these signals to produce images, magnetic field gradients ( $G_x$ ,  $G_y$ , and  $G_z$ ) are employed. Typically, the region to be imaged is scanned by a sequence of measurement cycles in which these gradients vary according to the particular localization method being used. The resulting set of received MR signals are digitized and processed to reconstruct the image using one of many well known reconstruction techniques.

In such MRI systems, the volume for acquiring MR data with optimal gradient linearity, having a uniform magnetic field  $B_0$ , and uniform radio frequency (RF) homogeneity is of limited extent. Desired fields-of-view (FOV) that exceed this limited volume are traditionally acquired in sections, with table motion between scans. The resulting concatenated images often exhibit discontinuities at the slab junctions. These slab-boundary artifacts result in non-ideal images. When these artifacts are either severe or occur in a critical region-of-interest, complete re-acquisition of data may be needed for a thorough analysis. In addition, the time for table motion extends scan time beyond that required for data acquisition.

Known methods designed to eliminate slab boundary artifacts in angiograms and 3D fast spin echo acquisitions include Sliding Interleaved  $k_y$  Acquisition (SLINKY) and Shifted Interleaved Multi-Volume Acquisition (SIMVA). These methods however, move the slab-selective excitation while keeping the table stationary rather than moving the table and keeping the slab position stationary. As a result, these methods are limited by the inherent optimal imaging volume of the MR scanner. These methods employ phase encoding in the z-direction and do not account for those situations where the z matrix is not equal to the number of  $k_x$ - $k_y$  subsets. Similarly, other known methods designed to

eliminate slab boundary artifacts have likewise moved the imaging slab rather than the patient table. Other known techniques implement a continuously moving table in both the phase encoding and frequency direction. However, prior techniques that move the patient table in the frequency-encode direction encode the data as if they were acquiring an image of the entire FOV and data is combined prior to any Fourier transform.

Other known systems employ stepped table and/or moving table approach with an array of receiver coils that move with the imaged object. Data is collected from each coil independently as it moves through the homogeneous volume of the scanner. None of these known systems however, collect data from a slab thickness that is fixed relative to the magnet, place the frequency encoding axis in the direction of table motion, and combine the data after Fourier transforming in the direction of table motion.

It would therefore be desirable to have a new method and apparatus that allows coverage of large FOV without slab-boundary artifacts in the resulting concatenated images.

### BRIEF DESCRIPTION OF THE INVENTION

The present invention relates to a system and method of acquiring large FOV MR images using continuous table motion for increased volume coverage that results in reconstructed images without discontinuities.

Slab-boundary artifacts are eliminated and scan time is reduced in an acquisition sequence by continuously moving an imaging object with respect to the optimal volume of the imaging apparatus, or vice versa. The thickness of the slab, which is smaller than the desired FOV, is selected to remain within the optimal volume of the MR system. The selected slab position remains fixed relative to the magnet of the MR scanner during the scan, and the table is moved continuously during scanning of the entire FOV. MR data is acquired by applying an excitation that excites spins and applying magnetic field gradient waveforms to encode the volume of interest. The volume of interest is restricted in the direction of table motion. The magnetic field gradients traverse k-space following a trajectory that is uniform in the k-space dimension that is in the direction of table motion. The magnetic field gradient waveforms that encode the k-space directions perpendicular to table motion are divided into subsets. During each acquisition, all the k-space data in the direction of table motion are acquired for a subset of at least one other k-space dimension. After acquisition, data is transformed in the direction of table motion, sorted, and aligned to match anatomical locations in the direction of table motion. This procedure is repeated to fill the entire matrix. A final image is reconstructed by transforming the data in the remaining dimension(s) perpendicular to table motion. This approach provides reconstructed images absent of slab-boundary artifacts over a large FOV and reduces the time needed for image acquisition.

In accordance with one aspect of the invention, a method of imaging large volumes without resulting slab-boundary artifacts includes defining a desired FOV larger than an optimal imaging volume of an MR scanner and selecting a slab thickness in a first direction that is smaller than the desired FOV but that is within the optimal imaging volume of the MR scanner. MR data is then acquired by exciting and encoding spins to acquire data that is restricted to the selected slab thickness. The imaging object is then moved continuously with respect to the imaging area, or vice versa. This process is repeated until the desired FOV is fully encoded using a series of cyclically repeated magnetic field

3

gradient waveforms. The selected trajectory need only be uniform in the direction of motion.

In accordance with another aspect of the invention, an MRI apparatus is disclosed to acquire multiple sets of MR data with a moving table and reconstruct MR images without slab-boundary artifacts that includes a magnetic resonance imaging system having an RF transceiver system and a plurality of gradient coils positioned about a bore of a magnet to impress a polarizing magnetic field. An RF switch is controlled by a pulse module to transmit and receive RF signals to and from an RF coil assembly to acquire MR data. A patient table is moveable fore and aft in the MR system about the magnetic bore to translate the patient so that an FOV larger than the optimal scanning area of the MRI system can be scanned. A computer is programmed to receive input defining a desired FOV larger than the optimal imaging volume of the MR system. The computer is also capable of defining a fixed slab with respect to the magnet to acquire the MR data therein. The computer then acquires full MR data using frequency encoding in the direction of table motion for a subset of the data in the direction(s) perpendicular to table motion while repositioning the patient table and maintaining the position of the fixed slab. The algorithm is repeated, collecting the necessary MR data across the defined FOV. The patient table can be tracked using the acquired MR data. To reconstruct the image, the MR data is first transformed in the direction of table motion, and then interpolated and aligned to match anatomic locations across slab boundaries. Thereafter, the MR data is transformed with respect to the remaining dimension(s) to reconstruct an MR image.

Yet another aspect of the invention includes a computer program having a set of instructions executed by a computer to control a medical imaging scanner and create large FOV images without significant boundary artifacts. The computer is caused to select an FOV spanning an area greater than a predefined optimal image area of the medical imaging scanner, apply an RF pulse to excite a region of interest, and apply magnetic field gradients to encode the region of interest in a first direction. The volume of interest is limited in the direction of table motion by acquiring the data in such a way that an acquisition filter can be used to restrict the spatial extent. Image data can then be acquired in the first direction as a subset of remaining direction(s) for each acquisition. The computer causes a patient table to move continually with respect to the medical imaging scanner, and repeat the image data acquisition with encoding in the first direction for the encoding in remaining direction(s) until sufficient data is acquired across the entire FOV. An image can be reconstructed without slab-boundary artifacts after aligning anatomical data in the first direction.

Various other features, objects and advantages of the present invention will be made apparent from the following detailed description and the drawings.

#### BRIEF DESCRIPTION OF THE DRAWINGS

The drawings illustrate embodiments presently contemplated for carrying out the invention.

In the drawings:

FIG. 1 is a schematic block diagram of an MR imaging system for use with the invention.

FIG. 2 is a diagram illustrating one embodiment of a data acquisition technique in accordance with the invention.

FIG. 3 is a diagram similar to FIG. 2, illustrating another embodiment for data acquisition in accordance with the invention.

4

FIG. 4 is a flow chart demonstrating a data acquisition algorithm for use with that shown in FIGS. 2 and 3.

FIG. 5 is a flow chart showing the data processing steps employed either during or after the data acquisition of FIG. 4.

FIG. 6 is a plot of a number of acquisitions versus total z-FOV for four values of slab thickness.

FIG. 7 is a plot of total scan time versus total z-FOV for the four values of slab thickness plotted in FIG. 6.

FIG. 8 is a diagram illustrating another embodiment of a data acquisition technique in accordance with the invention.

FIG. 9 is a flow chart demonstrating a data acquisition algorithm for use with that shown in FIG. 8.

FIG. 10 is a flow chart showing the data processing steps employed either during or after the data acquisition of FIG. 9.

FIG. 11 is a flow chart representing a data acquisition algorithm in accordance with an alternate embodiment of the invention.

#### DETAILED DESCRIPTION OF THE PREFERRED EMBODIMENT

Referring to FIG. 1, the major components of a preferred magnetic resonance imaging (MRI) system 10 incorporating the present invention are shown. The operation of the system is controlled from an operator console 12 which includes a keyboard or other input device 13, a control panel 14, and a display 16. The console 12 communicates through a link 18 with a separate computer system 20 that enables an operator to control the production and display of images on the screen 16. The computer system 20 includes a number of modules which communicate with each other through a backplane 20a. These include an image processor module 22, a CPU module 24 and a memory module 26, known in the art as a frame buffer for storing image data arrays. The computer system 20 is linked to disk storage 28 and tape drive 30 for storage of image data and programs, and communicates with a separate system control 32 through a high speed serial link 34. The input device 13 can include a mouse, joystick, keyboard, track ball, touch activated screen, light wand, voice control, or any similar or equivalent input device, and may be used for interactive geometry prescription.

The system control 32 includes a set of modules connected together by a backplane 32a. These include a CPU module 36 and a pulse generator module 38 which connects to the operator console 12 through a serial link 40. It is through link 40 that the system control 32 receives commands from the operator to indicate the scan sequence that is to be performed. The pulse generator module 38 operates the system components to carry out the desired scan sequence and produces data which indicates the timing, strength and shape of the RF pulses produced, and the timing and length of the data acquisition window. The pulse generator module 38 connects to a set of gradient amplifiers 42, to indicate the timing and shape of the gradient pulses that are produced during the scan. The pulse generator module 38 can also receive patient data from a physiological acquisition controller 44 that receives signals from a number of different sensors connected to the patient, such as ECG signals from electrodes attached to the patient. And finally, the pulse generator module 38 connects to a scan room interface circuit 46 which receives signals from various sensors associated with the condition of the patient and the magnet system. It is also through the scan room interface circuit 46 that a patient positioning system 48 receives commands to move the patient to the desired position for the scan.

The gradient waveforms produced by the pulse generator module **38** are applied to the gradient amplifier system **42** having Gx, Gy, and Gz amplifiers. Each gradient amplifier excites a corresponding physical gradient coil in a gradient coil assembly generally designated **50** to produce the magnetic field gradients used for spatially encoding acquired signals. The gradient coil assembly **50** forms part of a magnet assembly **52** which includes a polarizing magnet **54** and a whole-body RF coil **56**. A transceiver module **58** in the system control **32** produces pulses which are amplified by an RF amplifier **60** and coupled to the RF coil **56** by a transmit/receive switch **62**. The resulting signals emitted by the excited nuclei in the patient may be sensed by the same RF coil **56** and coupled through the transmit/receive switch **62** to a preamplifier **64**. The amplified MR signals are demodulated, filtered, and digitized in the receiver section of the transceiver **58**. The transmit/receive switch **62** is controlled by a signal from the pulse generator module **38** to electrically connect the RF amplifier **60** to the coil **56** during the transmit mode and to connect the preamplifier **64** to the coil **56** during the receive mode. The transmit/receive switch **62** can also enable a separate RF coil (for example, a surface coil) to be used in either the transmit or receive mode.

The MR signals picked up by the RF coil **56** are digitized by the transceiver module **58** and transferred to a memory module **66** in the system control **32**. A scan is complete when an array of raw k-space data has been acquired in the memory module **66**. This raw k-space data is processed as necessary and rearranged into separate k-space data arrays for each image to be reconstructed, and each of these is input to an array processor **68** which operates to Fourier transform the data into an array of image data. This image data is conveyed through the serial link **34** to the computer system **20** where it is stored in memory, such as disk storage **28**. In response to commands received from the operator console **12**, this image data may be archived in long term storage, such as on the tape drive **30** or any mass storage device, or it may be further processed by the image processor **22** and conveyed to the operator console **12** and presented on the display **16**.

The present invention includes a method and system suitable for use with the above-referenced MRI system, or any similar or equivalent system for obtaining MR images. When used with a trajectory that is uniform in the direction of table motion, such as z, data acquired in sections can be reconstructed to form large FOV images without significant slab-boundary artifacts.

As is known, in any MRI system, there is a limited spatial volume having optimal gradient linearity, uniform magnetic polarizing field  $B_0$ , and uniform RF homogeneity. Larger volumes are traditionally imaged in sections with table motion between scans that result in concatenated images that exhibit discontinuities at slab junctions.

One embodiment to generate large FOV images without slab-boundary artifacts includes a 3D imaging technique that steps the table position in increments during the scanning procedure. In general, after defining the desired FOV, a slab thickness is selected to remain within the MRI system's optimal imaging volume. As a result, the slab thickness is also smaller than the desired spatial coverage. MR data is acquired by repeatedly applying an excitation that excites spins and applying magnetic field gradient waveforms to encode the volume of interest. Preferably, a z slab selective RF pulse is used to excite the volume of interest in the z-direction and a 3D k-space trajectory encodes the volume selected. Some example of 3D k-space trajectories include a 3D EPI k-space trajectory, a cylindrical-stack of EPI k-space

trajectory, a stack-of-spirals k-space trajectory, a stack-of-TWIRL k-space trajectory, a stack-of-projection-reconstruction k-space trajectory, and a 3DFT k-space trajectory. More generally though, the spatial extent of the acquired data is restricted in the direction of motion using a method such as using a slab-selective RF pulse or by using an acquisition strategy that allows the acquisition filter to restrict the volume of interest. Therefore, in the examples shown and in a preferred embodiment, the direction of table motion is in the z-direction. However, as one skilled in the art will readily recognize, the x-y-z orientation is arbitrary and the invention is not so limited. In addition, in the example shown and in a preferred embodiment the table moves relative to the system. However, as one skilled in the art will readily recognize it is equivalent to have the system move relative to the subject and the invention is not so limited.

The table is moved to cover the desired FOV while the slab position remains fixed relative to the magnet in the MRI system. At each table position, full k-space data in the direction of table motion is acquired for a subset of the data in the other two dimension(s) by using one or a series of magnetic field gradient waveforms. In this embodiment, at each table position, full kz data is acquired for a subset of kx-ky by using one or a series of magnetic field gradient waveforms. Preferably, RF excitations and magnetic field gradient waveforms are continued during table motion to preserve a steady-state condition.

Referring to FIG. 2, a data acquisition and processing technique, in accordance with one embodiment of the invention, is shown schematically. FIG. 2 illustrates one embodiment of the invention for acquiring data. In this embodiment, the table is step-wise incremented 15 times with data acquisitions **106** in 16 table positions along the desired FOV. Each of the table increments are of equal distance  $\Delta z$ . A patient **100** is positioned on a moveable table **102**, which moves fore and aft **104** within the MRI scanner **10** with respect to the magnet and the optimal imaging area **108** of the MRI scanner. The desired FOV **110** is substantially larger than the optimal imaging area **108**, which is generally larger than a selected slab thickness **112**. As previously discussed, the table motion in this simplified example is in the z direction. Magnetic field gradient waveforms are designed to encode four kx-ky subsets ( $N_{wf}=4$ ) with a total of 16 table positions and data acquisition sets **106**. At each table position 1-16, there are four data acquisitions encoding four kz levels that result in four z-pixels in the excited slab after Fourier transformation in the z direction ( $N_z=4$ ).  $N_z$  and the retained slab thickness may be reduced slightly after acquisition if edge slices are dropped from each z-kx-ky data set to minimize the effect of imperfections in the slab profile. It is understood that the optimal imaging area **108** is defined by the physical characteristics of the MRI system **10**. It is preferred to define a volume of interest, or slab, **112** to be within the optimal imaging area **108**.

It is noted that when  $N_z=N_{wf}$ , each of the table increments throughout the desired FOV **110** are of equal distance. Accordingly, any of the aforementioned parameters can be adjusted as desired. That is, the slab thickness **114** may be made larger or smaller, or the number of table positions and data acquisition sets **106** can be increased or decreased, above or below the 16 that are shown. The minimum number of table positions desired to reconstruct an image is equal to the number of waveform subsets,  $N_{wf}$ . Additionally, the number of z-pixels,  $N_z$ , retained in each excited slab, as well as the number of kx-ky subsets can be modified as desired.

Preferably however,  $N_z$  is kept greater than or equal to  $N_{wf}$ . One such modification will be described with reference to FIG. 3.

Still referring to FIG. 2, it is noted that each table position 1–16, includes complete sampling in the direction of table motion which in this case is the z-direction, for a subset of the kx-ky data, or more generally, in the directions perpendicular to the direction of table motion. Accordingly, either after all the data at each table position is acquired, or after all the data is acquired for a complete image, the data is Fourier transformed in the direction of table motion, in this case in the z direction, FFT(z), to form an array of z-kx-ky data **120**. The patient table **102** is moved in steps until the entire FOV **110** is covered. As indicated, at each table position, full z-encoding data, or encoding data in the direction of table motion, is acquired for a subset of the kx-ky data, which are the two directions perpendicular to the table motion. While no data is acquired while the table is moving, it is desirable to continue the RF excitations and magnetic field gradient waveforms to preserve the steady-state condition.

After Fourier transforming with respect to z, or the direction of table motion, data acquired at different table positions are then sorted, interpolated as required, and aligned to match anatomic z locations, thereby filling the z-kx-ky space. In general, the table step distances are multiples of the z-resolution and are selected to ensure complete sampling of the z-kx-ky matrix. As previously indicated, after the acquired data are Fourier transformed with respect to z, data at the slab edges can be dropped as required by imperfections in the slab-select profile. A final reconstructed image **130** is formed by gridding, if necessary, and Fourier transforming the fully sampled data array **120** with respect to x and y.

For complete sampling, the number of z-pixels retained,  $N_z$ , must be at least equal to the number of kx-ky waveform subsets,  $N_{wf}$ . However, referring to FIG. 3, which also illustrates a simple example assuming table motion in the z direction, increasing the slab thickness **132** while maintaining the z resolution results in an increase in the number of z-pixels,  $N_z$ , that are encoded at each table position. In this example,  $N_z=8$  for 4 kx-ky subsets ( $N_{wf}=4$ ). Because  $N_z$  is greater than  $N_{wf}$ , the table increments are not all equal, as shown in FIG. 2. That is, the distance between table positions **1**, **2**, **3**, and **4**, is less than that between table positions **4** and table position **5**. Therefore, using a thicker slab, fewer movements of the table are required for the same spatial coverage. This results in an overall faster acquisition for the same size FOV, as compared to that in FIG. 2, if the time to initiate table motion is long relative to the time for a single acquisition. Even though increasing the slab thickness,  $N_z$ , incrementally increases individual acquisition time for each slab, the total scan time decreases because the time to initiate table motion dominates. Thus, in the case when the time to initiate table motion is long relative to the time for a single acquisition, scan time is minimized by minimizing the number of table movements. With current equipment, it typically takes approximately one second to initiate table motion. While reducing this time is the long-term desired solution, it is not practical in the short term since it requires significant changes to the system architecture.

Still referring to FIG. 3, after step-wise translating the patient table through the entire FOV **110** and acquiring data set **134**, the data is Fourier transformed with respect to z to obtain a z-kx-ky data set **136**. The data acquired at different table positions can then be sorted and aligned to match anatomic z locations. A final image **138** is reconstructed by

again first gridding, if necessary, and then Fourier transforming the fully sampled data with respect to x and y, FFT(xy).

To generalize, the table step distances are multiples of the pixel size in the direction of table motion and are selected to ensure complete sampling of the 3D matrix. The number of table steps required depends on the relative number of pixels retained in the excited slab,  $N_z$ , for the case of motion in the z direction, and the number of magnetic field gradient waveform subsets required to fully encode the dimension(s) perpendicular to table motion,  $N_{wf}$ . As previously indicated, for complete sampling,  $N_z$  should be at least equal to  $N_{wf}$ . However, if  $N_z$  is greater than  $N_{wf}$ , faster overall scan times are achievable. It is noted that the subsets of magnetic field gradient waveforms, (gx gy) are defined by one or a series of such waveforms that differ between subsets. This set, or series, of magnetic field gradient waveforms, that encode the kx, ky subsets, are then repeated in a cyclic manner to obtain the data sets **106**, FIG. 2, and **134**, FIG. 3.

The present technique can be used with any 3D k-space trajectory that is uniform in the direction of table motion. In one embodiment implemented on a system with table motion in the z direction, a cylindrical stack of EPI trajectory (CSEPI) sequence was utilized that phase encodes in kz between planes of interleaved EPI waveforms that are clipped to a circle in kx-ky. The data is gridded before Fourier transformation in x and y. The waveforms were designed with  $G_{max}=22$  mT/m and a slew rate of 120 mT/m/ms. Since k-space data for a single anatomic location is being compiled from data collected at different table positions, any variation in phase or amplitude in the direction of table motion will result in image artifacts. To minimize such artifacts, one embodiment uses a linear phase slab-select RF pulse with sharp transitions and low in-slice ripple, for example 0.5%, and drops one slice at each slab edge. Frequency variations in the direction of table motion that result from magnetic field inhomogeneity are demodulated during reconstruction. Further, decreasing the slab thickness also decreases the sensitivity to such variations.

FIG. 4 is a flow chart for a data acquisition sequence in accordance with the techniques of FIGS. 2 and 3. After the data acquisition sequence is initialized **140**, the table is positioned at the first location and a variable i is initialized **142**. MR data is acquired by repeatedly exciting spins using an RF pulse and applying magnetic field gradient waveforms to encode the volume of interest **144**. Assuming table motion in the z-direction, all kz data are acquired for the selected kx-ky subset, that are in the dimension(s) perpendicular to table motion **146**. The spatial extent in the direction of table motion is restricted using a restriction method such as either a slab-selective RF excitation or by acquiring data in such a way that the acquisition filter can be used to restrict the slab thickness. It is noted that for phase encoding in the direction of table motion the RF pulse is repeatedly applied prior to each acquisition **147** until all kz data is acquired **146**. For readout in the direction of table motion, each RF pulse is applied at **144** followed by acquisition of complete kz data for the selected kx-ky subset **146**. As long as the end of the FOV is not reached **148**, **150**, the variable i is incremented **152** and the system checks whether a complete set of magnetic gradient field waveform subsets has been acquired **154**. That is, as long as the variable i is not an even multiple of  $N_{wf}$  **154**, **156**, the table is moved a distance equal to the resolution in the direction of table motion **158**, and the next slab becomes the current slab at **144** and data is again acquired at **146**. After a complete series of subsets have been acquired **154**, **160**, the system determines if the next table



increment is in accordance to that described with reference to FIG. 2 or FIG. 3. That is, if the number of magnetic gradient field waveforms is equal to the number of pixels retained in the slab in the direction of table motion ( $N_{wf} = N_z$ ), the table is moved a distance equal to the z-resolution, or in the direction of table motion 162, as in FIG. 2, and the data acquisition sequence continues 144, 146. Otherwise, where  $N_z$  is greater than  $N_{wf}$  162, such as in FIG. 3, the table is moved a distance according to:

$$(N_z - N_{wf} + 1) \times (\text{z-resolution}), \quad \text{Eqn. 1}$$

and data is again acquired for the new slab 144, 146, until all the slabs have been scanned across the FOV 148, 168 which completes the scan at 170. Again, the direction of table motion is arbitrarily chosen and represented as a z-direction. However, the invention is not so limited. As one will readily recognize, the assignment of any character set can be used to represent a three dimensional axis.

It is noted that at each table position such as the acquisition at table position 1 in FIGS. 2 and 3, unique magnetic gradient waveforms or a set of waveforms on the gradient axes perpendicular to the direction of table motion (transverse waveforms) are applied in conjunction with the gradient waveform or waveforms required to acquire a complete set of data in the direction of table motion. At table positions 2, 3, and 4, different magnetic gradient field waveforms or sets of waveforms are applied on the axes perpendicular to the direction of table motion. The next series of table positions, 5-8, FIGS. 2 and 3, use the same magnetic field gradient waveforms as in the data acquisitions 1-4. Therefore, the variable  $i$  is used to also increment the application of the proper magnetic field gradient waveforms for the series, and when a series is complete, the same waveforms are recycled in the next series.

Referring now to FIG. 5, a data processing scheme in accordance with the present invention is shown in flow chart form. Once initiated 180, which can either be as data is being acquired on-the-fly, or after all data has been acquired, the MR data is Fourier transformed in the direction of table motion,  $z$  in this case, at 182, and if necessary, the data is corrected for shim errors in that direction 184. After Fourier transformation, the data at the edge boundaries of the slab are discarded as required 186, which results in  $N_z$  data elements in the direction of table motion. The data is then aligned to match anatomic locations at 188 and then, if necessary, the data may be gridded and corrected for shim errors in the remaining two directions at 190. The data is then Fourier transformed in the transverse dimension(s) at 192 to reconstruct the final image 194.

FIG. 6 is a graph plotting a number of acquisitions versus total FOV in the direction of table motion for three values of slab thickness and a single acquisition. In this exemplary acquisition having 18 transverse magnetic field gradient subsets and 1 mm resolution in the direction of table motion, the baseline 200 represents a single acquisition (i.e., no table movement), with the entire FOV acquired as a single large volume. The rippled line 202 shows the acquisition for a 1.8 cm slab, while the next plot 204 shows that for an 8 cm slab, and the largest stepped plot 206 is that for a 30 cm slab. Referring to FIG. 7, the total scan time for each of the acquisitions of FIG. 6 are shown plotted against total FOV in the direction of table motion in centimeters. Plot 210 corresponds to the 1.8 cm. slab acquisition, which took the longest total scan time because of the many table movements, while plot 216 is that of the single acquisition, which was the fastest. Between plots 210 and 216, the acquisition times for the 8 cm slab are shown by plot 212 and

the 30 cm slab by plot 214. Each of these acquisitions assumes 32 ms for each repetition of excitation plus acquisition of encoded data and one-second for each table movement. In this example, where the time to initiate table motion is long relative to the time required for a single acquisition, it is evident that the larger the slab thickness, the faster the scan times that can be achieved since fewer table motions are required.

In another embodiment, the present invention includes a process and system suitable for use with the MRI system of FIG. 1, or any similar or equivalent system, for obtaining MR images using frequency encoding in a direction parallel to continuous table motion, typically defined as the  $z$ -direction. Continuously moving the patient table allows for data acquisition at different table positions along the desired FOV with reduced scan time requirements. Collecting images while continuously moving the patient table and placing the frequency encoding axis in the direction of table motion has a number of advantages including the acquisition of images with FOV larger than the optimal imaging volume of the MR system, final reconstructed images that do not exhibit slab boundary artifacts, and less time associated with moving the patient table through the imaging volume. The present invention also allows for varying the repetition interval of excitation, gradient waveforms, and acquisitions with velocity. Further, any trajectory in the transverse  $k$ -space dimension(s) may be used. For example, for a 3D acquisition, the phase encodes could be positioned in the transverse  $k$ -space plane in the shape of a spiral, in concentric rings, in rays from the center, or in a Cartesian grid. For all positions other than the Cartesian grid, gridding of the data in the transverse plane occurs before performing the 2D Fourier transform.

Moreover, the present invention allows for acquisition of slightly over half of the full  $k$ -space data in the transverse dimension(s) with reconstruction using homodyne processing. Further, slightly over half of the full  $k$ -space data may be acquired in the readout direction, i.e., frequency encoded direction, which is in the direction of table motion. In addition, phase encodes in the transverse  $k$ -space dimension (s) may be acquired in any temporal order and/or with different temporal frequencies. For example, phase encodes closest to the  $k$ -space origin could be acquired with a higher temporal frequency than the phase encodes further from the  $k$ -space origin. Furthermore, a subset of phase encodes may be acquired during movement of the table over the FOV during forward movement of the patient table and then acquiring a different subset of phase encodes in the same FOV during reverse table direction. For example, low spatial frequency  $k$ -space lines may be acquired during a first pass over the FOV to acquire one time point of time-varying contrast and then acquire remaining phase encoding lines while the patient table is continuously moved back over the FOV.

Additionally, the present invention allows for acquisition of MR data for a larger slab thickness in the direction of continuous table motion than is used for image reconstruction. The data corresponding to the extra slab thickness may be selected so that data on subsequent repetitions of the same phase encoding would have overlapping coverage in the direction of table motion. This overlapping data may be used to estimate table velocity and position and/or other correction factors. Further, this overlapping data may be acquired using the same polarity of readout gradient or an opposite polarity. It may also have the same or different echo time. Data for the extra slab thickness may be acquired for all phase encodes or only the phase encode at the origin of the

k-space in the transverse dimension(s). The acquired MR data may also be used for creating an image as well as for estimating correction factors, or may be used as an extra acquisition that is used to estimate the correction factors. For example, MR data corresponding to the  $k_x=k_y=0$  line may be acquired with double the imaging slab thickness for each repetition of the full set of waveforms. From that, change in table position may be determined by performing a cross-correlation.

The present invention also enables the use of less data than acquired in the direction of table motion thereby allowing the dropping of data at a leading and a trailing edge of acquisition to combat imperfections in filtering. Estimations of imperfections in the magnetic field and center frequency induced by the magnet alone may be determined before starting table motion. Despite continuous table motion, these imperfections will be fixed relative to the magnet. Imperfections induced by object-dependent susceptibility will be superimposed on these fixed errors. The present invention is applicable with any type of image contrast including proton density, T1 weighted, T2 weighted, phase contrast, and SFFP type sequences. Saturation bands may be applied superior and/or inferior to the imaging slab to suppress inflowing blood from one or both directions or to create a different unique contrast effect. Further, the present invention allows for application of echo-planar type readouts in the direction of table motion to acquire different lines in k-space or, depending upon the application, reacquire the same k-space line. Such data may be used for image formation or it may be used to determine correction factors and/or table positions/velocity. If different k-space lines are acquired, the acquisition order may be linear or interleaved. The present invention also allows for correcting gradient non-linearities in a direction of table motion on each acquired line and for transverse gradient non-linearities by correcting each  $k_x$ - $k_y$  location individually based on the gradient non-linearity at the table location at the time of acquisition.

As is known and previously stated, in any MRI system, there is a limited spatial volume having optimal gradient linearity, uniform magnetic polarizing field  $B_0$ , and uniform RF homogeneity. Larger volumes are traditionally imaged in sections with table motion between scans that result in concatenated images that exhibit discontinuities at slab junctions. The present invention includes an imaging technique that moves the table position continuously during the scanning procedure to create large FOV images without slab boundary artifacts and without adding scan time for table motion between fixed-location acquisitions. Acquired images can be 2D single-slice, 2D multi-slice, 2D projection, or 3D.

In general, after defining the desired FOV, a slab thickness is selected to remain within the MRI system's optimal imaging volume. As a result, the slab thickness is also smaller than the desired spatial coverage. MR data is acquired by repeatedly applying an excitation that excites spins and applying magnetic field gradient waveforms to encode the volume of interest. Preferably, the spatial extent of the acquired data is restricted in the direction of motion using applied magnet field gradient waveforms that allow the acquisition filter to restrict the slab thickness. The FOV can be restricted using spatially-selective RF pulses in directions perpendicular to the direction of table motion. In the examples shown and in one preferred embodiment, the direction of continuous table motion is in the z-direction. However, as one skilled in the art will readily recognize, the x-y-z orientation is somewhat arbitrary and the invention is

therefore not so limited. In addition, in the example shown and in a preferred embodiment the table moves relative to the system. However, as one skilled in the art will readily recognize it is equivalent to have the system move relative to the subject and the invention is accordingly not so limited.

The table is moved to cover the desired FOV while the slab position remains fixed relative to the magnet in the MRI system. During each acquisition, full k-space data representing the selected slab in the direction of table motion is acquired for a subset of the data in the other dimension(s) by using one or a series of magnetic field gradient waveforms.

Referring to FIG. 8, the basic concepts of a data acquisition and processing technique, in accordance with this embodiment of the present invention, is shown schematically. FIG. 8 illustrates one embodiment of the present invention for acquiring data. In this embodiment, the table is moved continuously with 16 exemplary data acquisitions **306** at different table positions along the desired FOV. The table position and/or velocity at each acquisition is measured or estimated. A patient **300** is positioned on a moveable table **302**, which moves fore and aft **304** within the MRI scanner **10** with respect to the magnet and the optimal imaging area **308** of the MRI scanner. The desired FOV **310** is substantially larger than the optimal imaging area **308**, which is generally larger than a selected slab thickness **312**. As previously discussed, the table motion in this simplified example is in the z direction. Magnetic field gradient waveforms are designed to encode the full kz data for four k-space positions or subsets in the transverse dimension(s) ( $N_{wf}=4$ ). During each data acquisition **1-16**, four kz levels are encoded that result in four z-pixels in the excited slab after Fourier transformation in the z direction ( $N_z=4$ ).  $N_z$  and the slab thickness may be reduced after acquisition if data at the edges of the acquisition are dropped to minimize the effect of imperfections in the filter or for other reasons to be discussed below. It is understood that the optimal imaging area **308** is defined by the physical characteristics of the MRI system **10**. It is preferred to define a volume of interest, or slab, **312** to be within the optimal imaging area **308**.

Any of the aforementioned parameters can be adjusted as desired. That is, the slab thickness **314** may be made larger or smaller and the number of data acquisitions **306** can be increased or decreased, above or below the 16 that are shown. The maximum table velocity is determined by the slab thickness divided by the time required to collect all the data corresponding to one cycle through the set of gradient waveforms. Additionally, the number of z-pixels,  $N_z$ , retained in each excited slab, as well as the number of gradient waveforms in a set,  $N_{wf}$ , can be modified as desired.

Still referring to FIG. 8, it is noted that each acquisition position **1-16**, includes complete sampling in the direction of table motion which in this case is the z-direction, for a subset of the data in the direction(s) perpendicular to the direction of table motion. Accordingly, either after each acquisition, or after all the data is acquired for a complete image, the data is Fourier transformed in the direction of table motion, in this case in the z direction ( $FFT(z)$ ), to form an array of z-ktransverse data **320**. The patient table **302** is moved continuously until the entire FOV **310** is covered. As indicated, at each acquisition position, full z-encoding data, or frequency encoding data in the direction of table motion, is acquired for a subset of the desired transverse k-space positions, which are in the one or two directions perpendicular to the table motion.

After Fourier transforming with respect to z, or the direction of table motion, data acquired at different table

positions are then sorted and aligned to match anatomic z locations, thereby filling the z-ktransverse space. Data can be interpolated as necessary to improve the accuracy of the alignment. As previously indicated, after the acquired data are Fourier transformed with respect to z, data at the slab edges can be dropped as required by imperfections in filter performance or for other reasons as described below. A final reconstructed image **330** is formed by gridding and/or performing other processing as necessary, and Fourier transforming the fully sampled data array **320** in remaining dimension(s).

It is noted that the subsets of magnetic field gradient waveforms, ( $g_x$ ,  $g_y$ ,  $g_z$ ) are defined by one or a series of such waveforms that differ between subsets. This set, or series, of magnetic field gradient waveforms, that encode the ktransverse subsets, are then repeated in a cyclic manner to obtain the data sets **306**, FIG. **8**.

The present technique can be used with any 2D or 3D k-space trajectory that is uniform in the direction of table motion. For example, a 2D or 3D acquisition could be performed with the frequency-encoding axis in the direction of table motion and phase encoding gradients positioned on a Cartesian grid in the k-space dimension(s) that are perpendicular to the direction of table motion. Phase encoding gradients for a 3D acquisition could also be positioned on concentric circles, in the shape of a spiral, in rays from the center of k-space, or in any other pattern. In a 2D or 3D acquisition, phase encoding gradients could be placed in a pattern with density that varies with k-space position. If a non-Cartesian and/or non-uniform placement of ktransverse locations is utilized, the data would be gridded in the transverse dimension(s) during reconstruction.

Partial k-space techniques could be employed. For partial k-space in the transverse direction(s), slightly more than half of the data is acquired in the transverse direction. Homodyne processing would then be utilized in the reconstruction. Partial k-space techniques could also be used in the direction of table motion. Homodyne processing could also be used in this case.

Echo-planar type acquisitions could be employed with readout in the direction of table motion. This would allow full k-space data in the direction of table motion to be acquired for multiple transverse k-space positions following each RF excitation. Alternatively, full k-space data in the direction of table motion could be acquired multiple times for the same transverse k-space position following a single RF excitation. Such data acquisition could allow for the calculation of image correction factors.

Different k-space locations in the transverse dimension(s) may also be acquired with different slab thicknesses in the direction of table motion and therefore could be acquired with different temporal frequency during table motion.

As another variation, k-space locations in the transverse dimension(s) can be acquired in a variety of orders to achieve different modulations of k-space or different contrast properties. K-space locations in the transverse dimension(s) may be acquired sequentially from one edge of k-space to the other, centrally from the center out, in an interleaved fashion, or in any other pattern that is desired.

K-space locations in the transverse dimension(s) could also be divided into an arbitrary number of subsets that could be acquired in multiple table passages. For example, you could acquire the ktransverse data in two stages. First, you could acquire the ktransverse locations within a certain radius of the center of k-space. Since less time would be required to acquire this subset of the required data, the table could move faster over the selected FOV. As an example

application, this would allow the center of k-space, which has the largest impact on image contrast, to be acquired at the point of optimal contrast following administration of an extrinsic MR contrast agent. The table would then be moved back over the same FOV again to acquire higher spatial frequency k-space data.

As another extension, data for a larger selected slab thickness could be acquired in the direction of table motion. The extra data could be acquired for all transverse k-space positions or only some positions, for example the  $k_x=k_y=0$  line. The extra slab thickness could be selected such that the acquired data on subsequent repetitions of the same gradient waveform set would acquire data from overlapping spatial regions. This overlapping data could be used to estimate the distance of table motion between the two acquisitions or could be used to estimate other image correction factors. A portion of the data from these acquisitions with the increased slab thickness could be used to reconstruct the image in the normal fashion described in FIG. **8** or these acquisitions could be extra acquisitions that are interspersed between the standard acquisitions in the imaging experiment. The acquisitions with overlapping data could have identical imaging parameters or could have different echo times or readout gradients.

Since k-space data for a single anatomic location in the direction of table motion is compiled from data collected at different table positions, any variation in phase or amplitude in the direction of table motion will result in image artifacts. To minimize such artifacts, frequency variations in the direction of table motion that result from magnetic field inhomogeneity are demodulated during reconstruction. Frequency variations induced by the applied external magnetic field may be estimated before table motion begins. Gradient non-linearities can be corrected by assuming that these imperfections are separable between the direction of table motion and the transverse dimension(s). Gradient non-linearities in the direction of table motion are corrected for each data acquisition. Transverse non-linearities are corrected using a different factor for each transverse k-space location, or group of locations, that is/are determined using knowledge of the table position at the time of data acquisition. Signal phase induced by table motion during acquisition may be corrected during reconstruction.

FIG. **9** is a flow chart for a data acquisition sequence in accordance with the technique of FIG. **8**. After the data acquisition sequence is initialized **340**, selecting the 1st gradient waveform for each gradient axis ( $x$ ,  $y$ , and  $z$ ) occurs at **341**. The variable  $i$  represents the selected waveform for each axis. The table is positioned at a location superior or inferior to the desired FOV. In the preferred embodiment, this starting position is selected at **342** to allow the table to accelerate at **343** to the desired constant velocity before the leading edge of the desired FOV is reached. Alternatively, the starting position could be selected near the initial position requiring data to be acquired and the change in table velocity during acceleration could be accounted for in the data processing. MR data is acquired by repeatedly exciting spins using an RF pulse and applying magnetic field gradient waveforms to encode the volume of interest **344**. All RF and gradient waveforms would be played out even if data is not acquired during table acceleration to establish the steady-state MR signal levels. Assuming table motion in the  $z$ -direction, each acquisition would ensure all  $k_z$  data are acquired for the selected transverse k-space position(s), that is in the dimension(s) perpendicular to table motion ( $k_x$  and/or  $k_y$ ). The table position and/or velocity is measured or estimated and recorded for the time of data acquisition. The

spatial extent represented by the data in the direction of table motion is limited by acquiring data in such a way that the acquisition filter can be used to restrict the slab thickness. A determination is then made at **348** to determine if sufficient data to reconstruct the desired FOV has been acquired. As long as sufficient data to reconstruct the desired FOV has not been acquired **348**, **350**, the system checks whether a complete set of magnetic gradient field waveforms has been applied ( $I=Nwf$ ?) **351**. If a complete set of magnet gradient field waveforms have been applied **351**, **352**, the system again selects the 1st waveform on each axis at **353** and the cycle begins anew at **344**. If not, the system increments to the next gradient waveform **356** and data is acquired for the current slab position as the table continues to move **344**. This process is repeated until all the slabs have been scanned across the FOV **358**, which completes the scan **360**. Again, the direction of table motion is arbitrarily chosen and represented as a z-direction. However, the invention is not so limited. As one will readily recognize, the assignment of any character set can be used to represent a three dimensional axis.

It is noted that at each data acquisition position such as the acquisition at position **1** in FIG. **8**, unique magnetic gradient waveforms or a set of waveforms on the gradient axis perpendicular to the direction of table motion (transverse waveforms) are applied in conjunction with the gradient waveform or waveforms required to acquire a complete set of data in the direction of table motion. At positions **2**, **3**, and **4**, different magnetic gradient field waveforms or sets of waveforms are applied on the axis perpendicular to the direction of table motion. The waveform on the axis parallel to the direction of table motion can be the same for each set or can also vary. The next series of acquisition positions, **5-8**, FIG. **8**, use the same magnetic field gradient waveforms as in the data acquisitions **1-4**. Therefore, the variable  $i$  is used in FIG. **9** to increment the application of the proper magnetic field gradient waveforms for the series, and when a series is complete, the same waveforms are recycled in the next series.

Referring now to FIG. **10**, a data processing scheme in accordance with one embodiment of the present invention is shown in flow chart form. Once initiated **380**, which can either be as data is being acquired on-the-fly, or after all data has been acquired, the MR data is corrected for phase inducements caused by the table motion **381**. It is then Fourier transformed in the direction of table motion,  $z$  in this case, at **382**, and if necessary, the data is corrected for imperfections in the magnetic field and gradient non-linearities in that direction **384**. After Fourier transformation, the data at the edge boundaries of the slab and/or extra data are discarded as required **386**. Either after or during the Fourier transform, the data is aligned to match anatomic locations at **388**, interpolating as necessary. Then, some, all, or none of the following additional processing steps are performed as required by the specifics of the imaging procedure: the data may be gridded in the transverse dimension(s), corrected for shim errors in the transverse direction(s), homodyne processed in the transverse direction(s), and/or corrected for gradient non-linearities in the transverse dimension(s) at **390**. The data is then Fourier transformed in the transverse dimension(s) at **392** to reconstruct the final image **394**.

Referring to FIG. **11**, the steps of another embodiment of the present invention are shown in flow chart form. After the data acquisition sequence is initialized **400**, the transverse k-space waveforms are divided into  $N_s$  subsets of  $N_{wf}$  **402**. Subsets may be formed with unequal numbers of

waveforms, but for this simplified example each subset has an equal number of waveforms,  $N_{wf}$ . The first waveform of the first subset is then selected at **404**. The patient table is then positioned at a starting location **406** such that the table is allowed to accelerate to the desired constant velocity at **408** before the leading edge of the desired FOV is reached. MR data is then acquired by repeatedly exciting spins using an RF pulse and applying the  $J$ th gradient waveform of the  $I$ th subset on each gradient axis to encode the current slab and acquire all  $kz$  data for the relevant transverse k-space positions at **410**. At **412**, the process determines if sufficient data has been acquired for the selected subset to reconstruct desired FOV **412**. If not **412**, **414**, the process determines at **416** if the complete set of magnetic gradient waveforms have been applied ( $J=N_{wf}$ ). If so **416**, **418**, the process again selects the first waveform on each axis at **420** and the cycle begins anew at **410**. If not **416**, **422**, the process increments to the next gradient waveform **424** and data is acquired for the current slab position. This process is repeated until all slabs have been scanned across the FOV, which completes the scan in a first or forward direction.

If at **412**, the process determines that there is sufficient data acquired for the selected subset to reconstruct the desired FOV **426**, the process determines if the last subset has been encoded at **428**. If not **428**, **430**, the process increments the subset and resets the waveform, i.e.,  $J=1$  at **432**. At **434**, the table is decelerated to zero velocity and subsequently reversed and accelerated until a desired constant velocity is reached. An RF and  $J$ th gradient waveform of the  $I+1$  subset on each gradient axis are then applied at **410** while the table moves in a second or reverse direction. If at **428** the last subset has been encoded and sufficient data has been acquired to reconstruct a final image for the desired FOV **435**, the scan ends at **436**.

Methods such as those described here could be used to acquire images with a variety of contrast properties. As examples, images could display proton-density weighting, T1 weighting, T2 weighting, or any other weighting available in stationary-table imaging. Image contrast could be manipulated by interleaving the repetition of imaging RF and gradient waveforms with RF and gradient waveforms designed to saturate, invert, or otherwise manipulate spins in regions superior or inferior to the selected imaging slab or with specific spectral properties. Such saturation regions could suppress in-flowing materials from the direction saturated, could saturate lipid spins, or could achieve different contrast effects due to the movement of the patient table.

There are a number of advantages associated with the present invention. For example, the present invention allows for 3D imaging with continuous motion and frequency encoding in the direction of the patient and/or patient table motion. Two-dimensional single-slice or multi-slice imaging with continuous motion and frequency encoding in the direction of table motion is also possible. Further, 2D projection with continuous motion and frequency encoding in the direction of motion may be achieved with the present invention. The present invention further allows for different spatial distributions of phase encode positions such as spiral, concentric rings, variable density, etc. and using gridding reconstruction techniques. The present invention further allows for partial k-space imaging methods with continuous table motion as well as different phase encode orderings with continuous table motion. The present invention also enables for tracking of table position using acquired larger slab thickness in a direction of table movement thereby allowing for the overlapping of data. Additionally, the table may be

moved several times over a desired anatomy to achieve greater image quality. The present invention also allows for performing off-resonance and gradient linearity correction with moving table as well as using saturation bands with a moving table. EPI readout in a direction of table motion to either reacquire the same k-space line or a different line is possible with the present invention. Further, the present invention allows for different temporal update rates for different phase encode positions.

Accordingly, the present invention includes a method of imaging large volumes without resulting slab-boundary artifacts that includes defining a desired FOV larger than an optimal imaging volume of an MR scanner, selecting a slab thickness in a first direction that is smaller than the desired FOV, but within the optimal imaging volume of the MR scanner, then exciting and encoding spins to acquire data that is restricted to the selected slab thickness. MR data is acquired that includes full encoding data in the direction of table motion for a subset of the remaining direction(s) and continual moving one of the optimal imaging volume and an imaging object to acquire another set of MR data. This process of acquiring sets of MR data and continual moving the table is repeated until the desired FOV is covered. Acquired MR data can be used and analyzed to track motion of the table. In a preferred embodiment, each MR data acquisition includes acquiring all k-space data in the direction of table motion for a selected subset of the remaining transverse dimension(s), and further includes defining a set or series of magnetic field gradient waveforms that encode a k-space trajectory that is uniform in a k-space dimension (s) along the direction of movement.

The invention also includes an MRI apparatus, such as that disclosed with reference to FIG. 1, having a patient table moveable fore and aft in the MRI system within the magnet and a computer programmed to receive input defining a desired FOV larger than an optimal imaging volume of the MRI system. The MRI system comprises a plurality of gradient coils positioned about a bore of a magnet to impress a polarizing magnetic field, and an RF transceiver system and an RF switch controlled by a pulse module to transmit RF signals to an RF coil assembly to acquire MR images. The computer is programmed to define a fixed slab with respect to the magnet to acquire MR data and acquire full MR data using frequency encoding in the direction of table motion for a selected subset of data in the directions perpendicular to the direction of table motion. The patient table is moved while maintaining position of the fixed slab, and the system is further programmed to repeat the acquisition and movement until an MR data set is acquired across the desired FOV that is sufficient to reconstruct an image of the FOV.

Additionally, the present invention also includes a computer program to control a medical image scanner and create images across scanning boundaries without boundary artifacts. The computer program has a set of instructions to control a computer to select an FOV spanning an area greater than a predefined optimal imaging area of the medical image scanner and acquire MR data by repeatedly applying an RF pulse to excite a region in the selected FOV and magnetic field gradients to encode the region in a direction. The instructions further control the computer to apply a k-space trajectory to encode the region in the direction of table motion and acquire data for a subset of the remaining direction(s). The computer program includes instructions to continuously reposition the imaging object with respect to the predefined optimal imaging area or vice versa and repeat the image data acquisition and the continu-

ous imaging area repositioning until complete image data are acquired across the entire FOV to reconstruct an image of the FOV. Positioning of the optimal imaging area can be tracked using acquired MR data, or other known processes.

The present invention results in images that are free of slab-boundary artifacts, reduces the time required for data acquisition, and allows spatial coverage that is limited only by the range of table motion.

The present invention has been described in terms of the preferred embodiment, and it is recognized that equivalents, alternatives, and modifications aside from those expressly stated, are possible and within the scope of the appending claims.

What is claimed is:

1. A method of imaging large volumes without resulting slab-boundary artifacts, the method comprising:
  - defining a desired FOV larger than an optimal imaging volume of an MR scanner in at least a first direction;
  - defining desired phase encode locations in at least one dimension perpendicular to the first direction;
  - choosing a plurality of slab thicknesses in the first direction wherein slab thickness varies with each phase encode location and is smaller than the desired FOV and within the optimal imaging volume of the MR scanner; and
  - continuously moving one of the optimal imaging volume and an imaging object in the first direction while repeatedly exciting and encoding spins with readout in the first direction to acquire data that is restricted to a slab thickness for a set of phase encode locations until a set of MR data for the FOV for the first set of phase encode locations is acquired;
  - reversing the direction of motion of one of the optimal imaging volume and the imaging object in the first direction;
  - continuously moving one of the optimal imaging volume and the imaging object in the a reversed direction while repeatedly exciting and encoding spins with readout in the first direction to acquire data that is restricted to the slab thickness for a second set of phase encode locations until a set of MR data for the FOV for the second set of phase encode locations is acquired; and
  - reconstructing at least one image of the FOV from the set of MR data for the first set of phase encode locations and the set of MR data for the second set of phase encode locations.
2. The method of claim 1 wherein the phase encode locations are divided into a number of sets and wherein each set has a constant slab thickness.
3. The method of claim 1 further comprising acquiring multiple lines of data following a single excitation to minimize overall scan time.
4. The method of claim 1, further comprising selecting a set of phase encode locations to be proximate to a center of k-space in a transverse direction and timing acquisition of the set of phase encode locations to capture optimal image contrast associated with passage of a bolus of extrinsic contrast agent.
5. The method of claim 1 further comprising interleaving with a pre-defined temporal frequency between the exciting and encoding waveforms and alternate RF and gradient waveforms to manipulate image contrast.
6. The method of claim 5 further comprising alternate RF and gradient waveforms designed to manipulate spins in spatially localized regions relative to the slab.
7. The method of claim 1 further comprising acquiring MR data associated with multiple phase encode locations following a single excitation.

19

8. The method of claim 1 further comprising acquiring MR data associated with a single phase encode location multiple times following a single excitation.

9. The method of claim 1 further comprising acquiring MR data with different temporal frequencies for reconstructing an image and further comprising tracking a relative motion of the optimal imaging volume and the imaging object.

10. The method of claim 1 wherein acquiring MR data includes frequency encoding in the first direction.

11. The method of claim 1 further comprising reconstructing the at least one image of the FOV by:

altering a phase of the acquired MR data to correct for motion;

Fourier transforming the MR data in the first direction; and

sorting and aligning the transformed data to match anatomical locations.

12. The method of claim 11 further comprising reconstructing the at least one image of the FOV by transforming the MR data in remaining transverse dimension(s).

13. The method of claim 11 further comprising gridding and transforming the MR data in dimension(s) perpendicular to the first direction.

14. The method of claim 11 further comprising separately correcting each line of MR data for gradient non-linearities after transforming in the first direction.

15. A method of imaging large volumes without resulting slab-boundary artifacts, the method comprising:

defining a desired FOV larger than an optimal imaging volume of an MR scanner in at least a first direction;

defining desired phase encode locations in at least one dimension perpendicular to the first direction;

enabling readout in the first direction;

choosing a plurality of slab thicknesses in the first direction wherein slab thickness varies with each phase encode location and is smaller than the desired FOV and within the optimal imaging volume of the MR scanner; and

continuously moving one of the optimal imaging volume and an imaging object in the first direction while repeatedly exciting and encoding spins with readout in the first direction to acquire MR data that is restricted to a chosen slab thickness for the phase encode location being encoded until at least one image of the FOV can be reconstructed by:

altering a phase of the acquired MR data to correct for motion;

Fourier transforming the MR data in the first direction; gridding and transforming the MR data in at least one dimension perpendicular to the first direction; and

sorting and aligning the transformed data to match anatomical locations.

16. A computer readable storage medium having stored thereon a computer program to control a medical imaging device and create large FOV images without boundary artifacts, the computer program having a set of instructions that when executed by a computer causes the computer to:

define a desired FOV larger than an optimal imaging volume of an MR scanner in at least a first direction;

determine a slab in the first direction having a thickness that is smaller than the desired FOV and within the optimal imaging volume of the MR scanner;

define readout in a first direction;

select a set of phase encode locations to be proximate to a center of k-space in a transverse direction to the first

20

direction and timing acquisition of the set of phase encode locations to capture optimal image contrast associated with passage of a bolus of extrinsic contrast agent; and

continuously move one of the optimal imaging volume and an imaging object in the first direction while repeatedly exciting and encoding spins with readout in the first direction to acquire data that is restricted to the slab until at least one image of the FOV can be reconstructed.

17. The computer readable storage medium of claim 16 wherein the computer program has further instructions to cause the computer to acquire the data using frequency encoding in a direction of table motion.

18. The computer readable storage medium of claim 16 wherein the computer program has further instructions to cause the computer to:

alter a phase of the acquired MR data to correct for motion;

Fourier transform the data in the first direction; and sort and align the transformed data to match anatomical locations.

19. The computer readable storage medium of claim 18 wherein the computer has further instructions to separately correct each line of MR data for gradient non-linearities after transforming in the first direction.

20. The computer readable storage medium of claim 18 wherein the computer has further instructions to reconstruct an MR image by transforming the MR data in remaining transverse dimension(s).

21. The computer readable storage medium of claim 18 wherein the computer has further instructions to grid and then transform the MR data in dimension(s) perpendicular to the first direction.

22. The computer readable storage medium of claim 16 wherein the computer program has further instructions to cause the computer to track continuous movement of the optimal imaging volume with respect to the imaging object.

23. The computer readable storage medium of claim 16 wherein the computer program has further instructions to cause the computer to do at least one of:

apply an echo planar readout in a direction of table motion;

determine at least one of table position and table velocity; determine phase encode locations; and

determine a data acquisition order.

24. An MRI apparatus, to acquire multiple sets of MR data with a moving table and reconstruct MR images without slab-boundary artifacts, the apparatus comprising:

a magnetic resonance imaging (MRI) system having a plurality of gradient coils positioned about a bore of a magnet, and an RF transceiver system and an RF switch controlled by a pulse module to transmit RF signals to an RF coil assembly designed to acquire MR images; a patient table movable fore and aft in the MRI system within the magnet bore; and

a computer programmed to:

receive input defining a desired FOV larger than an optimal imaging volume of the MRI system in at least a first direction;

define desired phase encode locations in at least one dimension perpendicular to the first direction;

divide desired phase encode locations into sets;

choose at least one slab thickness in the first direction wherein slab thickness is constant for each set of phase

## 21

encode locations and is smaller than the desired FOV and within the optimal imaging volume of the MR scanner;

readout in the first direction:

continuously move one of the optimal imaging volume and an imaging object in the first direction while repeatedly exciting and encoding spins with readout in the first direction to acquire data restricted to the slab thickness for the defined phase encode locations until at least one image of the FOV can be reconstructed; and correct for gradient non-linearities.

25. The MRI apparatus of claim 24 wherein the computer is further programmed to transmit magnetic gradient waveforms to acquire data with frequency encoding in a direction of table motion.

26. The MRI apparatus of claim 24 wherein the computer is further programmed to:

transform MR data in the first direction;

align the transformed MR data to match anatomy across slab boundaries; and

transform the data with respect to at least one remaining dimension to reconstruct an MR image.

27. The MRI apparatus of claim 24 wherein the computer is further programmed to:

apply an RF pulse to excite a volume of interest;

apply a k-space trajectory to encode the volume of interest; and

filter the acquired MR data to restrict the MR data to the defined slab.

28. The MRI apparatus of claim 24 wherein the computer is further programmed to acquire MR data and track MR data using different temporal frequencies.

29. The MRI apparatus of claim 24 wherein the computer is further programmed to:

acquire k-space data for the first direction for a selected subset of transverse k-space data;

define a set of magnetic field gradient waveforms to incrementally encode and acquire data in a given slab; and

apply the set of magnetic field gradient waveforms in a cyclic order.

30. A method of imaging large volumes without resulting slab-boundary artifacts, the method comprising:

(A) defining a desired FOV larger than an optimal imaging volume of an MR scanner in at least a first direction;

(B) defining desired phase encode locations in at least one direction perpendicular to the first direction;

(C) dividing desired phase encode locations into sets;

(D) choosing at least one slab thickness in the first direction, wherein slab thickness is constant for each set of phase encode location and is smaller than the desired FOV and within the optimal imaging volume of the MR scanner;

(E) frequency encoding in the first direction;

(F) continuously moving one of optimal imaging volume and an imaging object in the first direction while repeatedly exciting and encoding spins with readout in the first direction to acquire data that is restricted to a slab thickness for a first set of phase encode locations until a set of MR data for the first set of phase encode locations is acquired for the entire FOV;

(G) reversing the direction of motion of one of the optimal imaging volume and the imaging object;

## 22

(H) continuously moving one of the optimal imaging volume and the imaging object in a reverse direction while repeatedly exciting and encoding spins with readout in the first direction to acquire data that is restricted to the slab thickness for a next set of phase encode locations until a set of MR data for the next set of phase encode locations is acquired; and

(I) reconstructing at least one image of the FOV from the acquired sets of MR data.

31. The method of claim 30 further comprising repeating (F) through (G) for each remaining set of phase encode locations until at least one image of the FOV can be reconstructed from the sets of MR data.

32. The method of claim 30 further comprising selecting a set of phase encode locations to be proximate to a center of k-space in a transverse direction and timing the acquisition of the set of phase encode locations to capture optimal image contrast associated with passage of a bolus of extrinsic contrast agent.

33. The method of claim 30 further comprising:

altering a phase of MR data to account for motion;

transforming the sets of MR data in the first direction; and

sorting, interpolating, and aligning the transformed sets of MR data to match anatomic locations in the first direction.

34. The method of claim 33 further comprising gridding and transforming the transformed MR data in dimension(s) perpendicular to the first direction to reconstruct an MR image.

35. The method of claim 33 further comprising reconstructing an MR image by transforming the transformed MR data in remaining transverse dimension(s).

36. An controller for imaging large volumes without resulting slab-boundary artifacts, the controller having a set of instructions that causes the controller to:

define a desired FOV larger than an optimal imaging volume of an MR scanner in at least a first direction, the desired FOV having a number of sets of phase encode locations;

choose at least one slab thickness in the first direction wherein the at least one slab thickness is constant for each set of phase encode locations and is smaller than the desired FOV and within the optimal imaging volume of the MR scanner;

frequency encode in the first direction;

translate one of the optimal imaging volume and an imaging object in the first direction while repeatedly exciting and encoding spins with a first combination of exciting and encoding waveforms and with readout in the first direction to acquire MR data that is restricted to a slab thickness of a phase encode location; and

interleave a pre-defined temporal frequency between the first combination of exciting and encoding waveforms with another combination of RF and gradient waveforms configured to excite and encode spins outside the slab thickness-until at least one image of the FOV can be reconstructed.

37. The controller of claim 36 wherein the set of instructions further causes the controller to interleave alternate combinations of RF and gradient waveforms to manipulate spins in spatially localized regions relative to the slab.

38. The controller of claim 36 wherein the set of instructions further causes the controller to interleave alternate combinations of RF and gradient waveforms to manipulate spins in a specific spectral range.

23

39. A system for imaging large volumes without resulting slab-boundary artifacts, the system comprising:

means for defining a desired FOV larger than an optimal imaging volume of an MR scanner in at least a first direction;

means for defining desired phase encode locations in at least one dimension perpendicular to the first direction;

means for dividing desired phase encode locations into sets; means for defining readout in the first direction:

means for choosing at least one slab thickness in the first direction, wherein slab thickness is constant for each set of phase encode locations and is smaller than the desired FOV and within the optimal imaging volume of the MR scanner; and

24

means for continuously moving one of the optimal imaging volume and an imaging object in the first direction while repeatedly exciting and encoding spins with readout in the first direction to acquire multiple lines of MR data following each excitation until at least one image of the FOV can be reconstructed.

40. The system of claim 39 further comprising means for acquiring MR data associated with multiple phase encode locations following each excitation.

41. The system of claim 39 further comprising means for acquiring multiple sets of MR data associated with a single phase encode location following each excitation.

\* \* \* \* \*